



ASYOD Eğitim Toplantıları 2019

İleri Mekanik Ventilasyon Uygulamaları Kursu



SOLUNUM MEKANİKLERİ: NASIL ÖLÇERİM?

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**Gazi Üniversitesi Tıp Fakültesi Göğüs Hastalıkları
Anabilim Dalı Yoğun Bakım Ünitesi**

09.11.2019

SOLUNUM MEKANİKLERİ

“Akciğer fonksiyonlarının basınç, akım, volüm ölçümleri ile ifade edilmesi”

SOLUNUM MEKANİKLERİ

- **Neden önemli?**

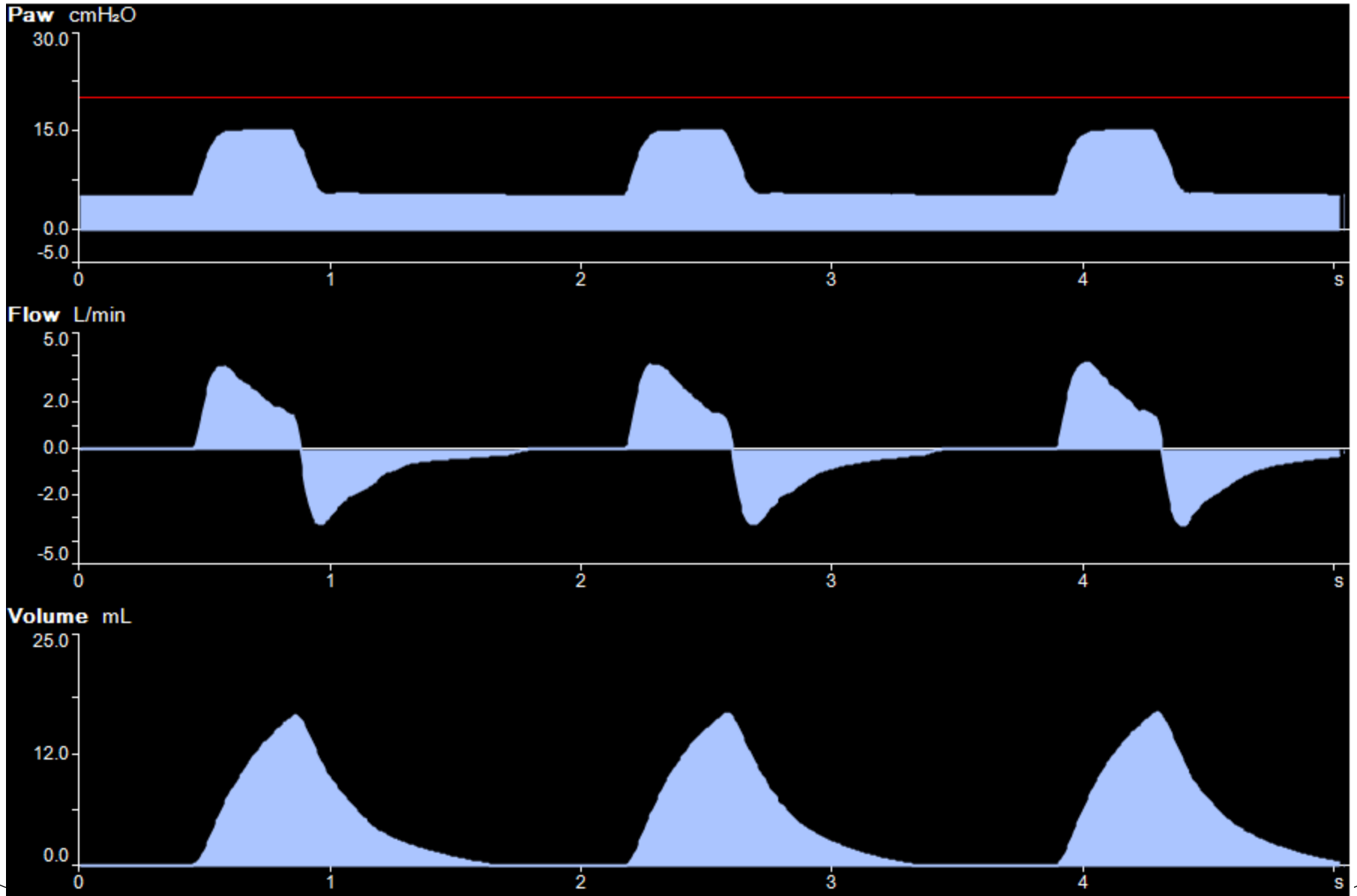
- Akut solunum yetmezliğinin altta yatan patofizyolojisini anlamak
- Hastalığın durumunu ve seyrini değerlendirmek
- Tedavi yaklaşımını belirlemek (PEEP, bronkodilatörler, sıvı tedavisi)
- Hasta ventilatör uyumunu sağlamak
- Ventilatör ilişkili komplikasyonları önlemek
- Mekanik ventilasyonun sonlandırılmasına karar verebilmek

SOLUNUM MEKANİKLERİNİ NASIL DEĞERLENDİRELİM?

Ventilatör Grafikleri:

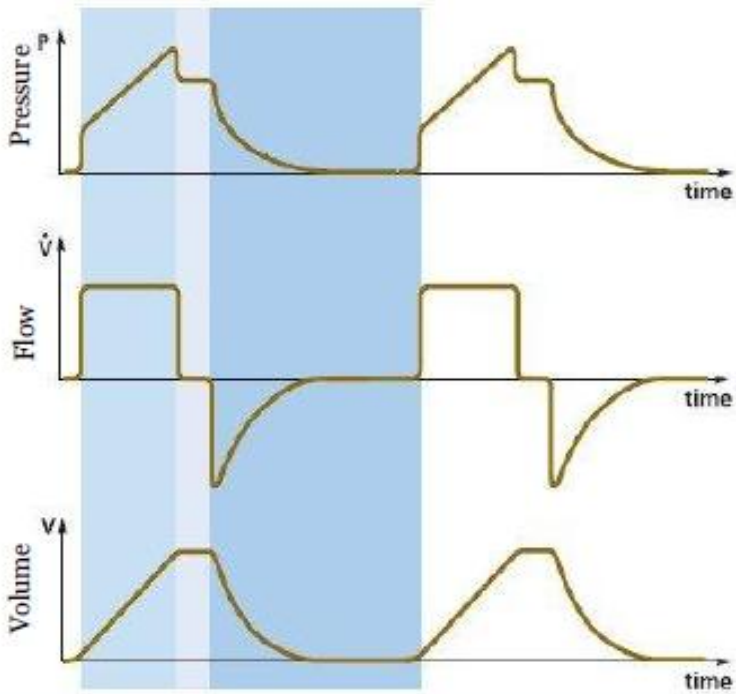
- Basınç, akım ve volüm eğrileri
- Özafageal (plevral) ve gastrik (abdominal) basınçlar
- Ölçümler
 - Komplians
 - Rezistans
- Zaman ilişkili grafikler (waveforms)
 - Basınç
 - Akım
 - Volüm
- Döngüler
 - Basınç volüm
 - Akım Volüm

BASINÇ-AKIM-VOLÜM EĞRİLERİ



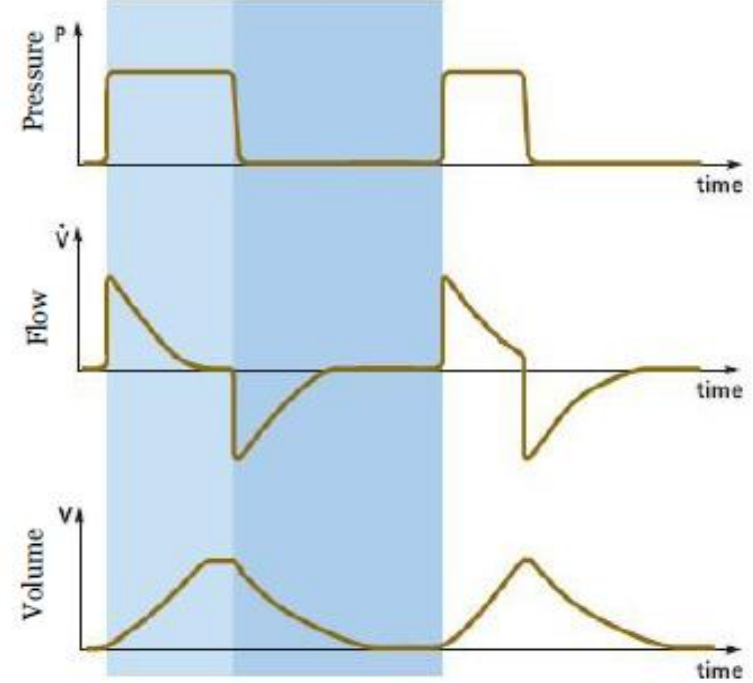
DALGA FORMLARI

Volume Modes



Volume Control
SIMV (Vol. Control)

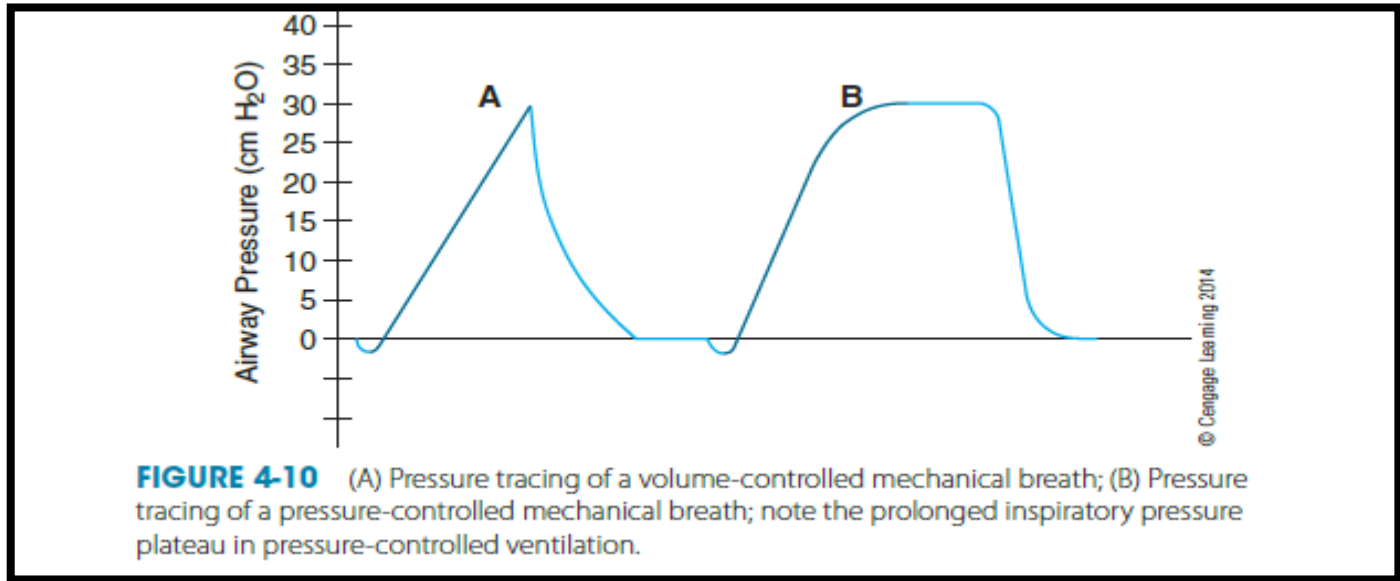
Pressure Modes



Pressure Control
PRVC
SIMV (PRVC)
SIMV (Press. Control)

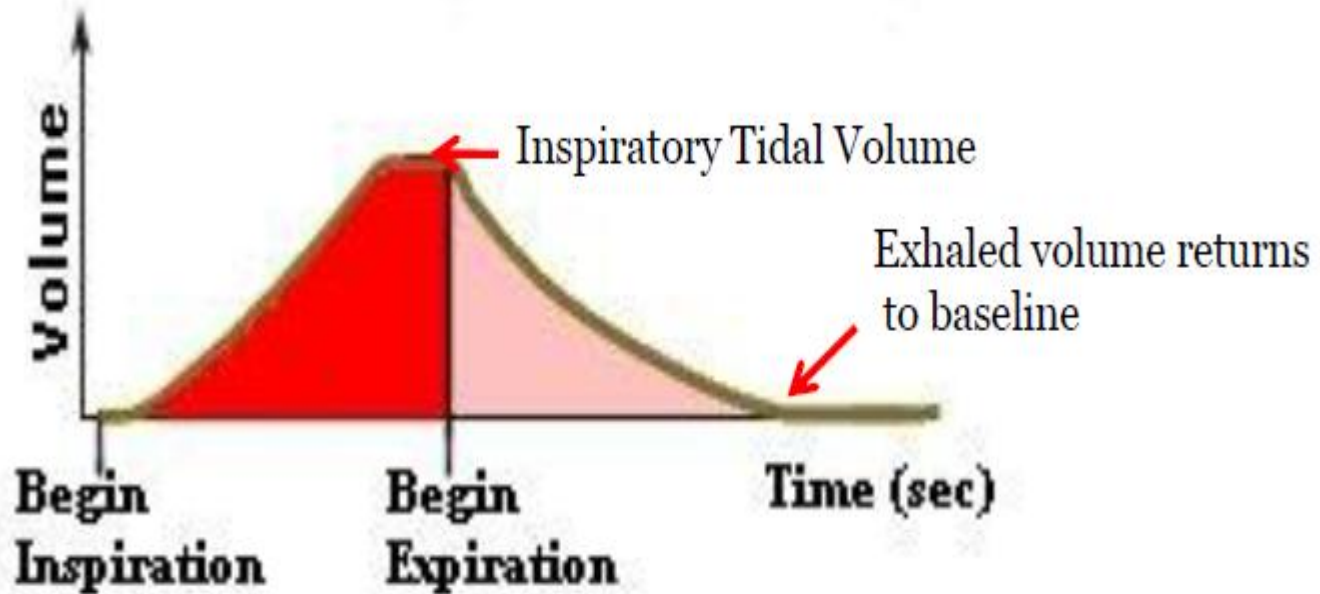
Pressure Support
Volume Support

BASINÇ DALGA FORMU

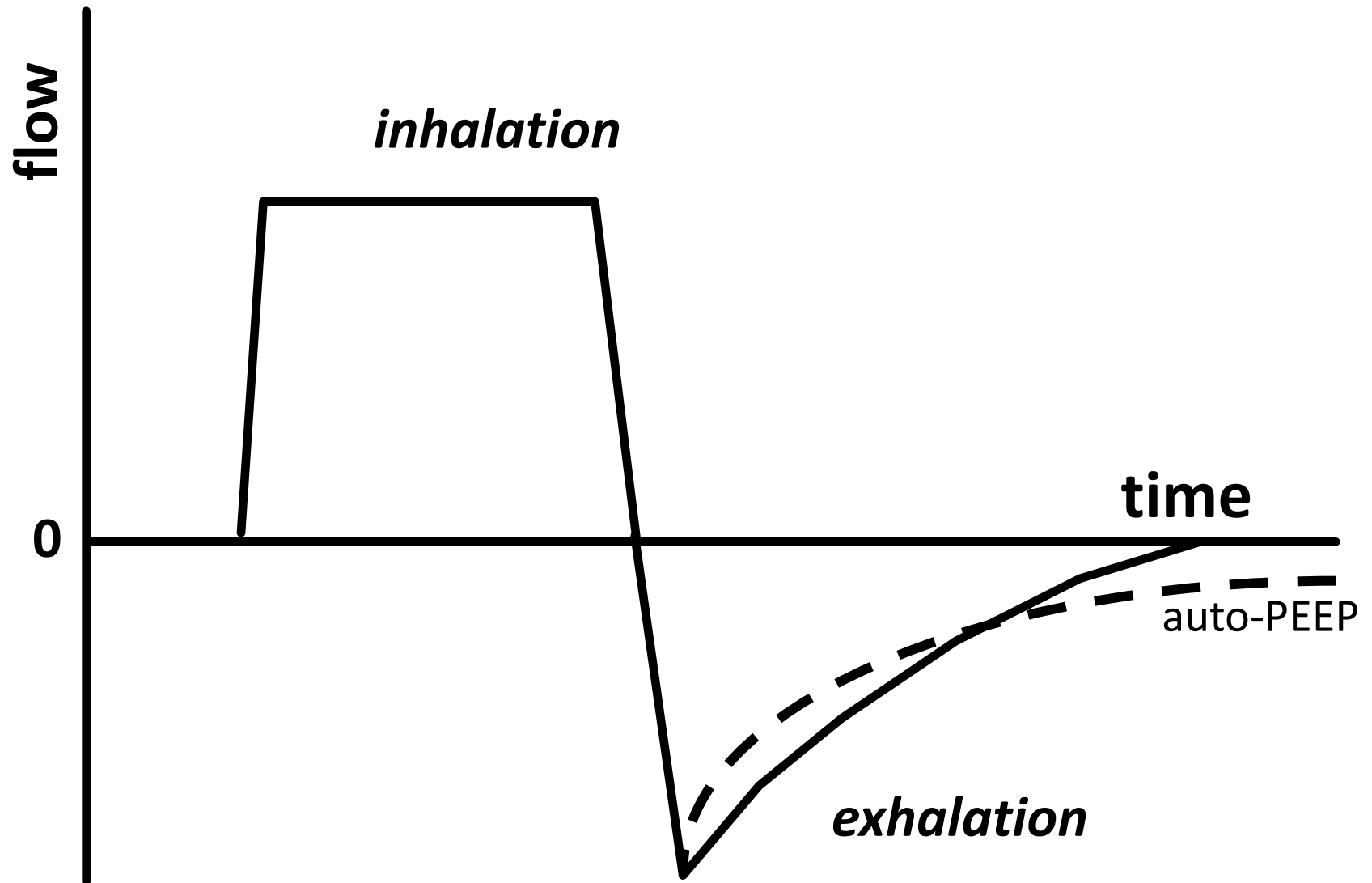


Clinical Application of Mechanical
Ventilation, Fourth Edition
David W. Chang

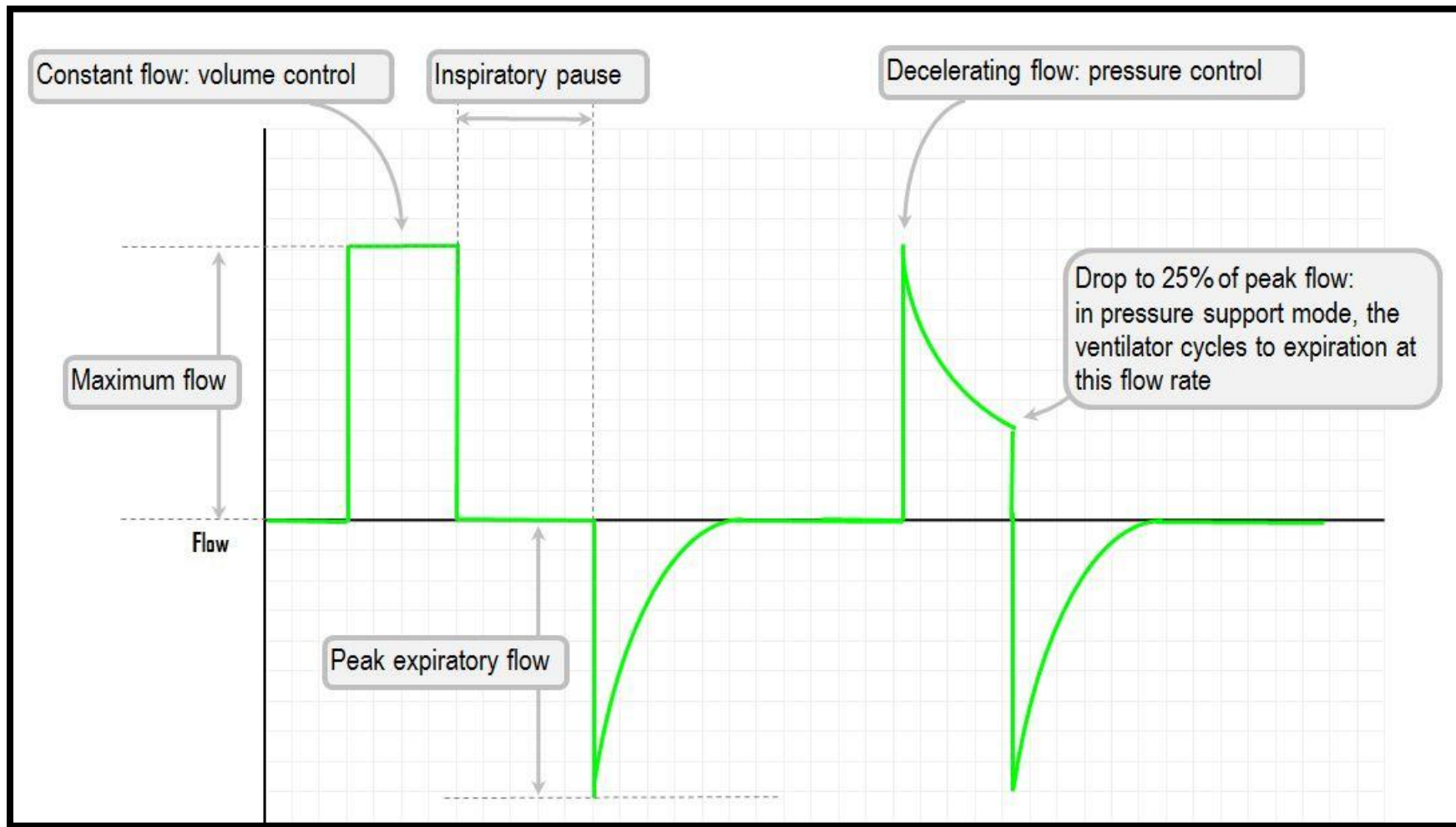
VOLÜM DALGA FORMU



AKIM DALGA FORMU



AKIM DALGA FORMU



ÖLÇÜMLER

(KOMPLİANS,ELASTANS,REZİSTANS,WOB)

SOLUNUM MEKANİKLERİ

KOMPLİANS

Volüm deęişikliği / Basınç deęişikliği

«Akcięerin genişleyebilme kolaylığı»

Belirli bir basınç artışına baęlı olarak oluşan hacim artışının ölçüsü (1/elastans)

SOLUNUM MEKANİKLERİ

ELASTANS (1/KOMPLİANS)

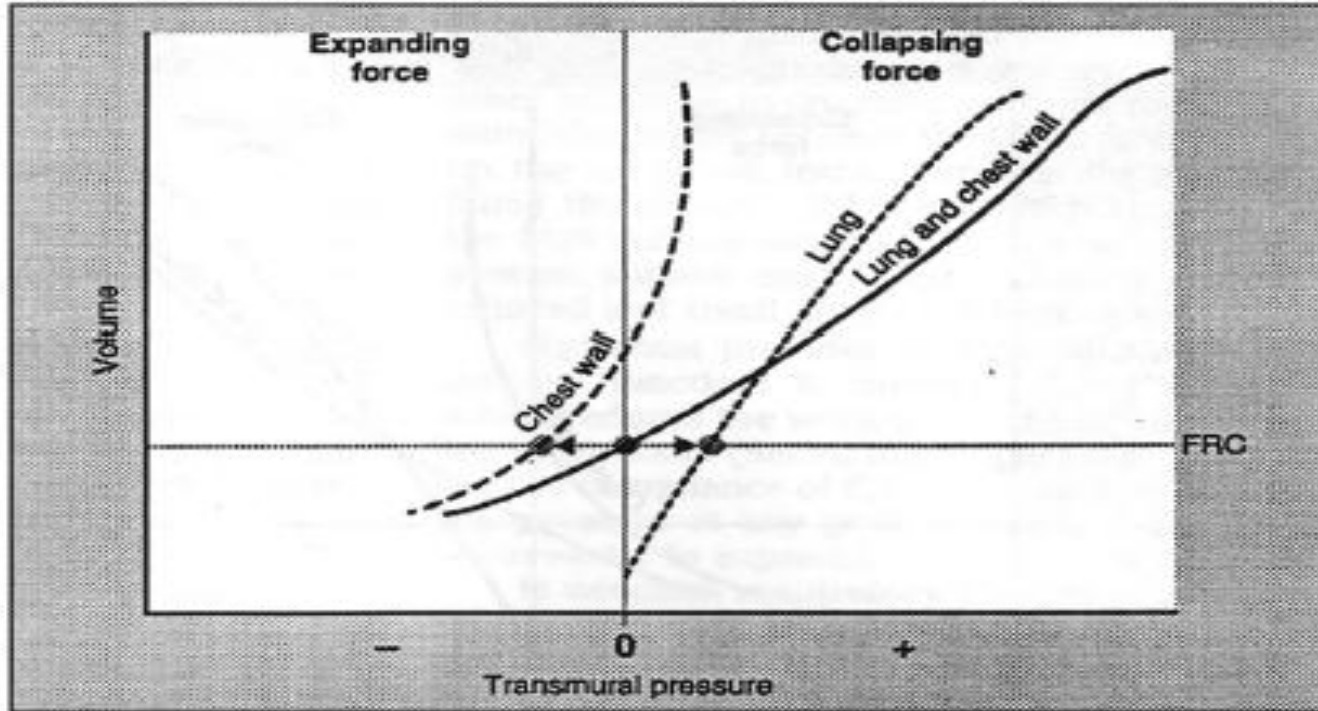
Volüm deęişikliği / Basınç deęişikliği

«Gerilen akcięerlerin eski řekline dönebilmesi»

Akcięerin elastik özellikleri (1/3)

Sıvı içerięinin yüzey gerilimi (2/3)

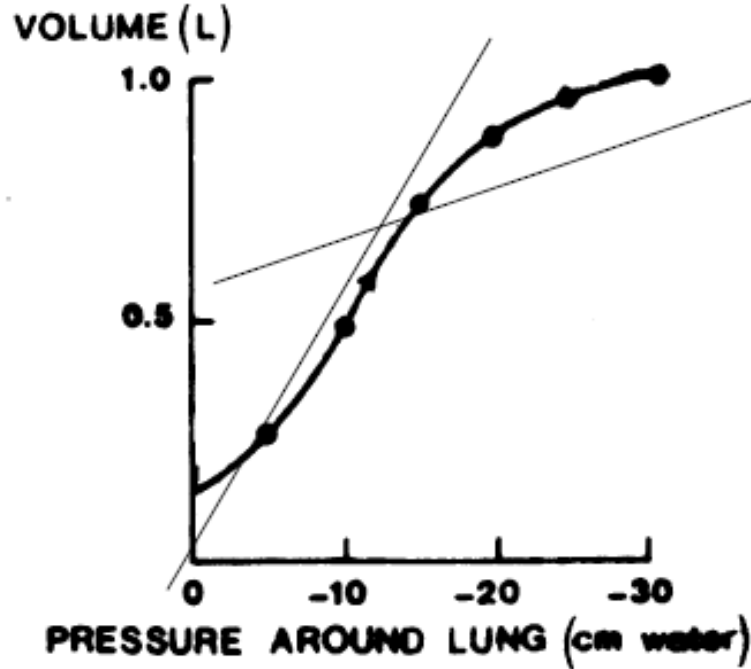
Figure 2



Compliance of the lungs, chest wall, and the combined lung–chest wall system. At the functional residual capacity, the forces of expansion and collapse are in equilibrium. Reprinted from [3] with permission from Elsevier.

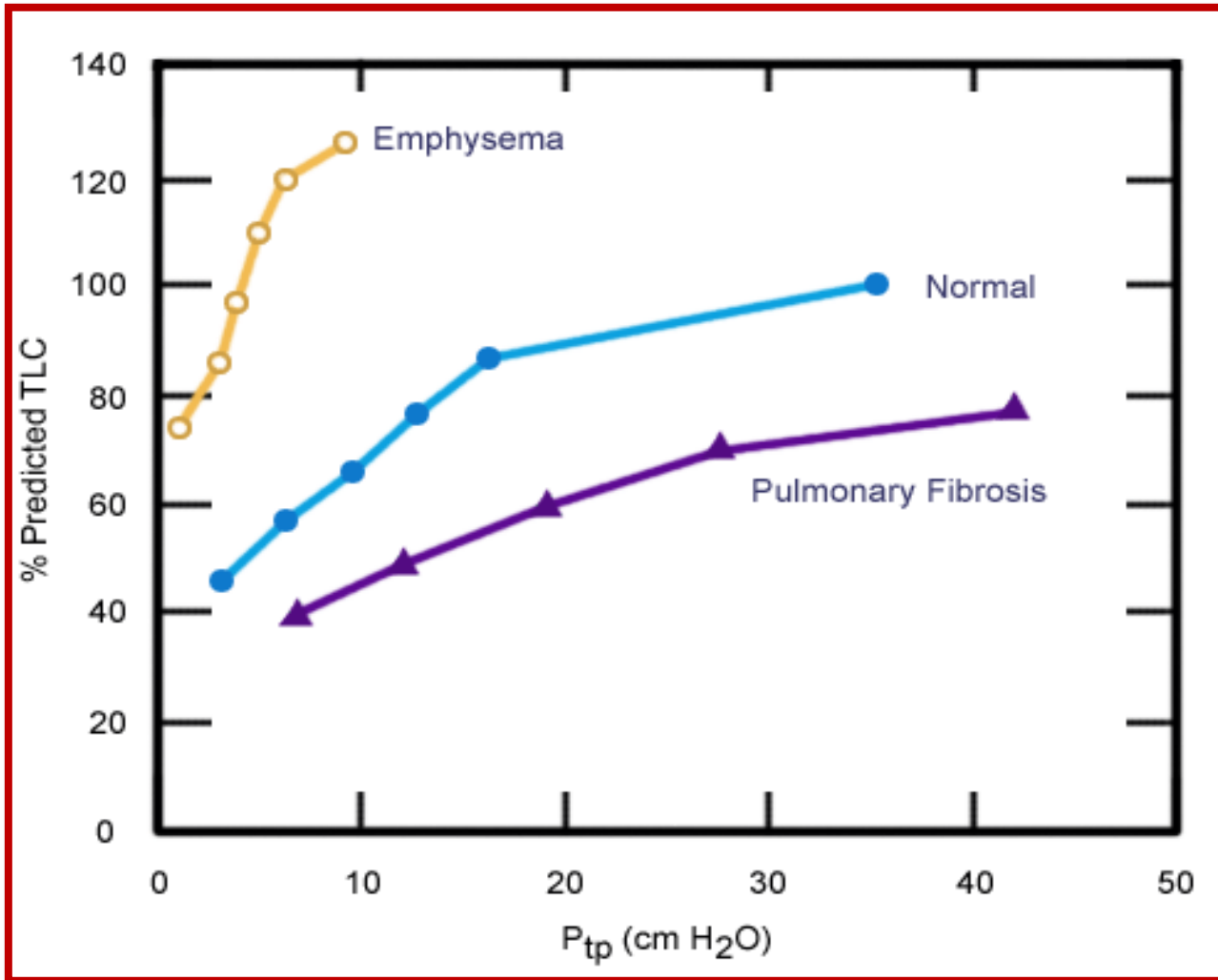
Normal toplam komplians:(akciğer+göğüs duvarı)= 200 ml/cm H₂O
Basınç 1 cmH₂O arttığında akciğerler 200ml genişler

AC'lerin kompliyansı

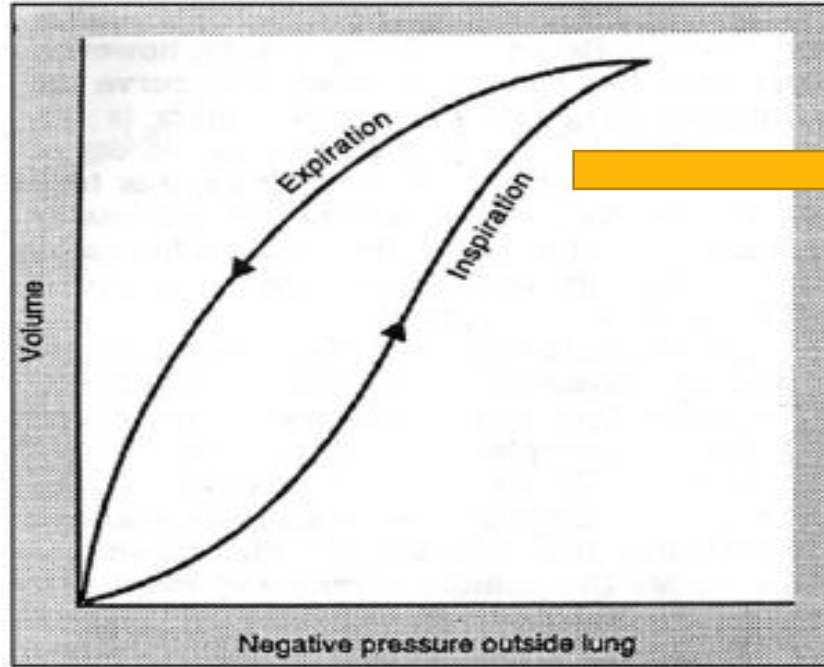


- Eğrinin dik olması yüksek kompliyansı, yatık olması düşük kompliyansı gösterir.
- Dolayısıyla AC kompliyansı yüksek volümlerde en düşük, rezidüel volüm seviyelerinde en yüksek noktasındadır.

KOMPLIANS



KOMPLİANS

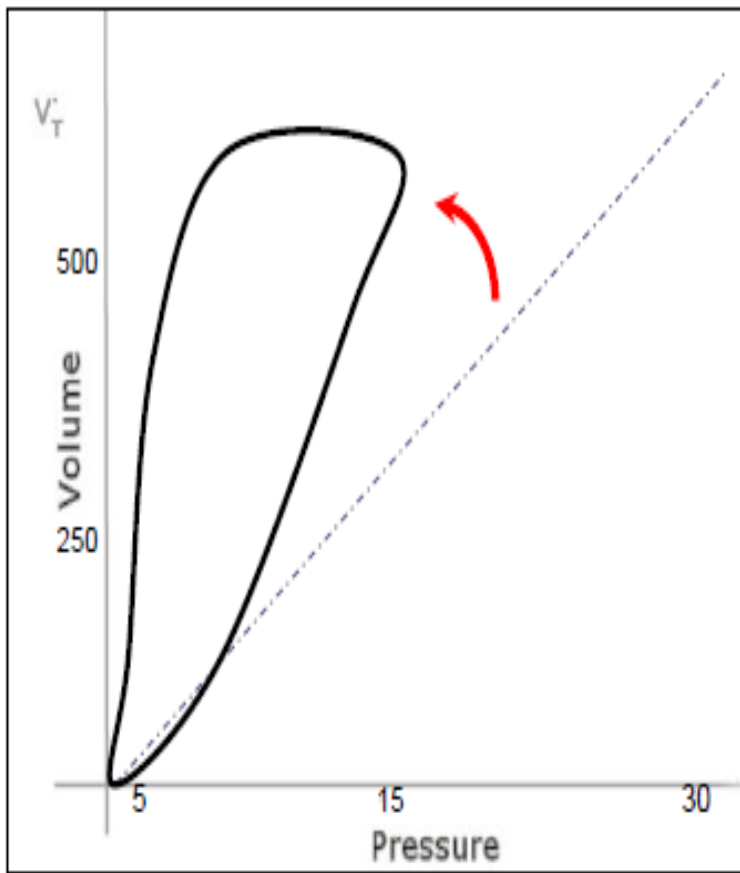


Histerezis; elastik yapılarda uygulanan kuvvet sonrası oluşan volüm değişikliğinin kuvvet ortadan kalktıktan sonra belirli bir zaman korunması

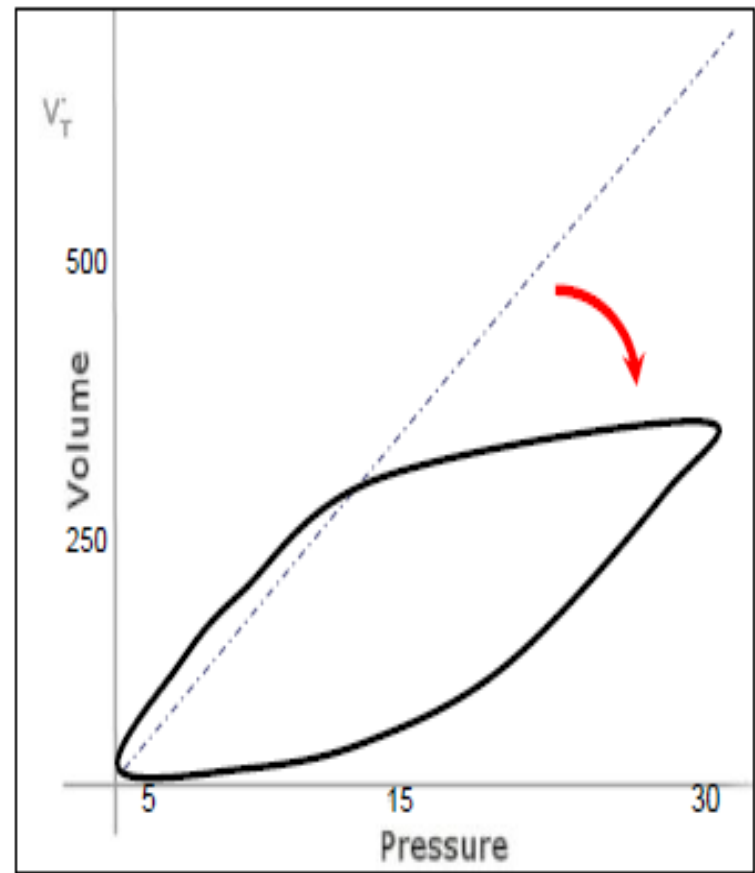
Pressure–volume curve. Shown is a pressure–volume curve developed from measurements in isolated lung during inflation (inspiration) and deflation (expiration). The slope of each curve is the compliance. The difference in the curves is hysteresis. Reprinted from [3] with permission from Elsevier.

P-V Eğrisi- Eğrinin eğimi kompliansı verir

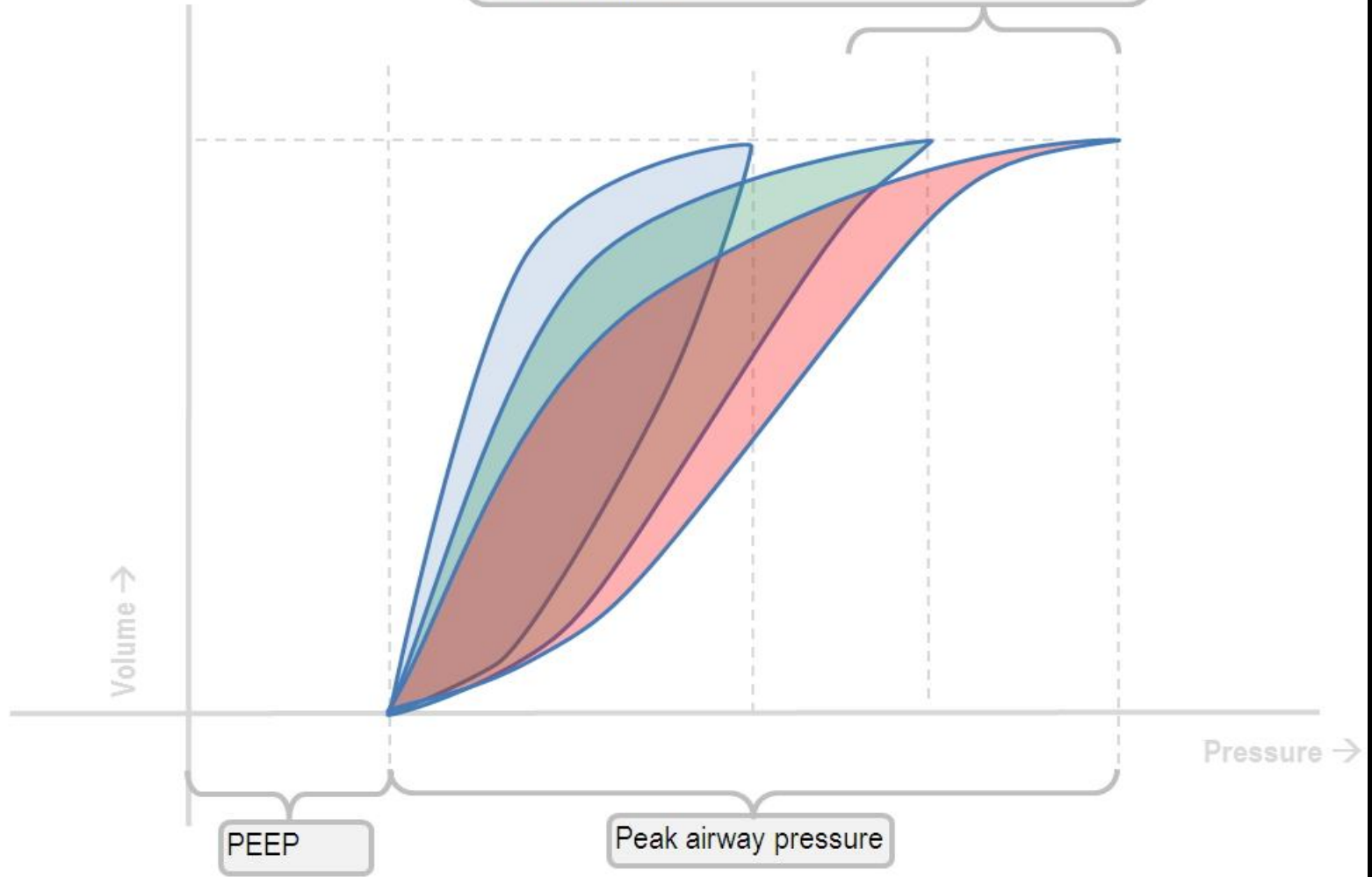
ARTMIŞ KOMPLİANS



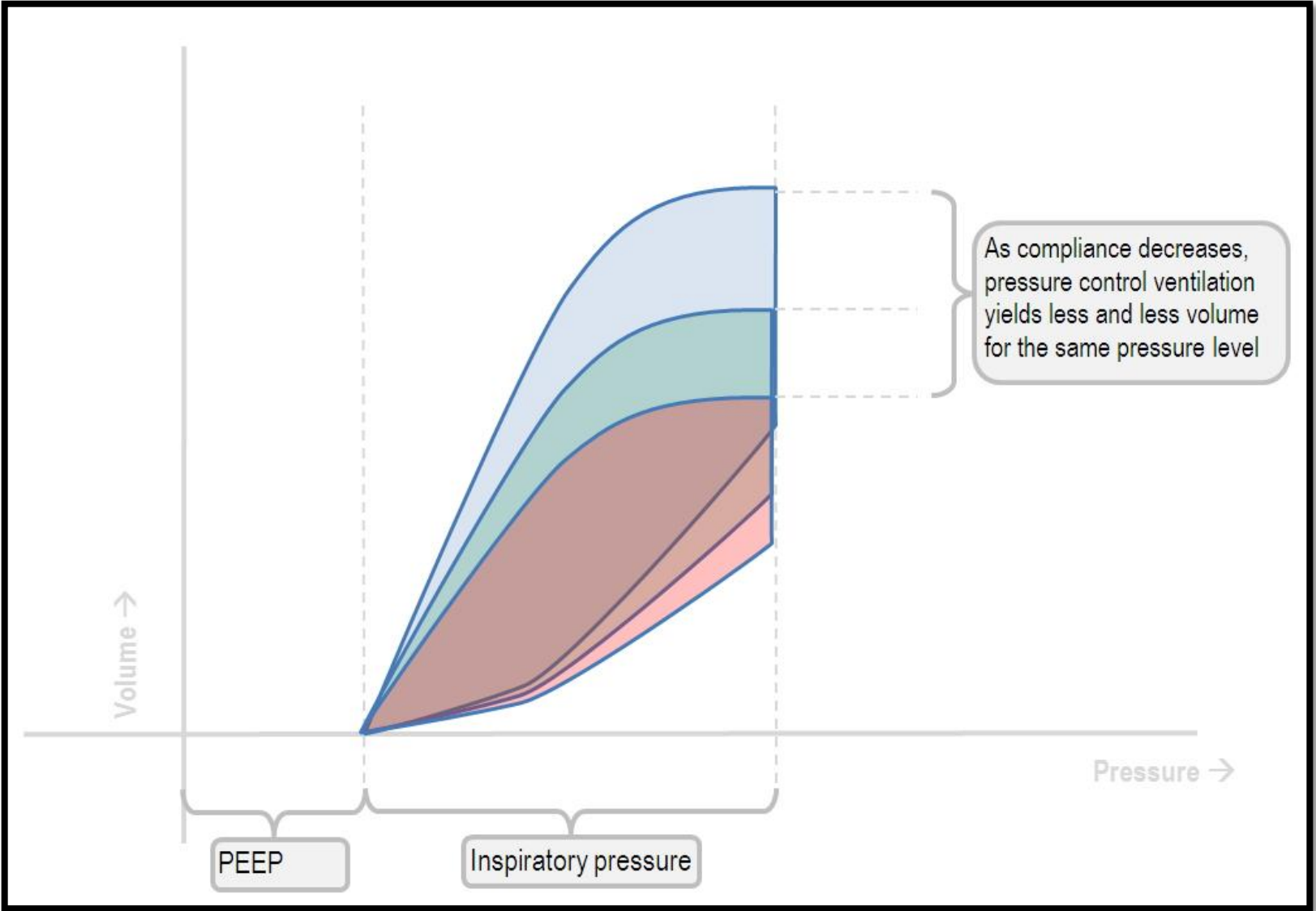
AZALMIŞ KOMPLİANS



As compliance decreases, volume control ventilation yields higher and higher peak airway pressure in order to achieve the same volume.

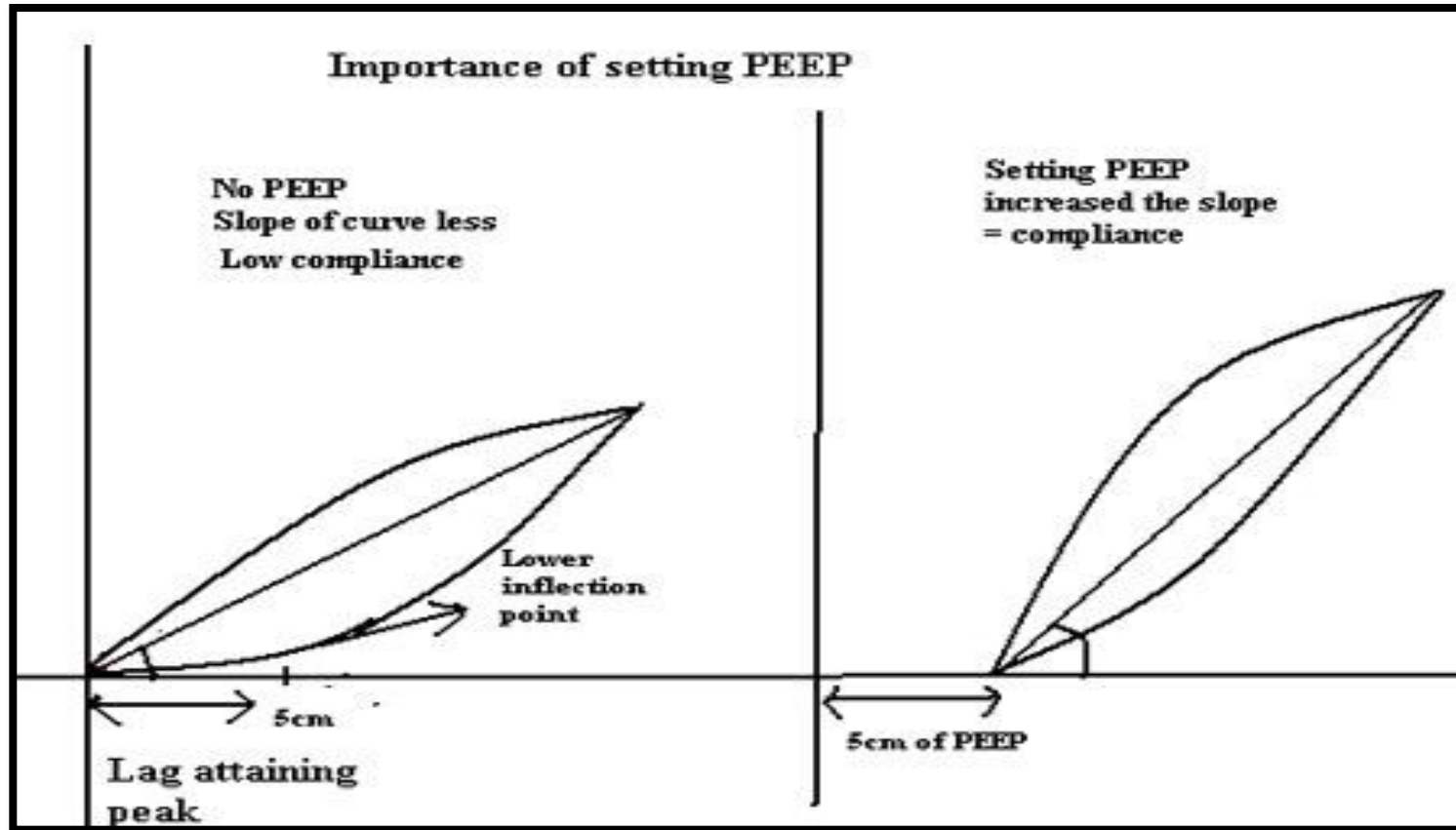


Volüm Kontrollü Ventilasyonda P-V Eğrisi ile Kompliansın Değerlendirilmesi



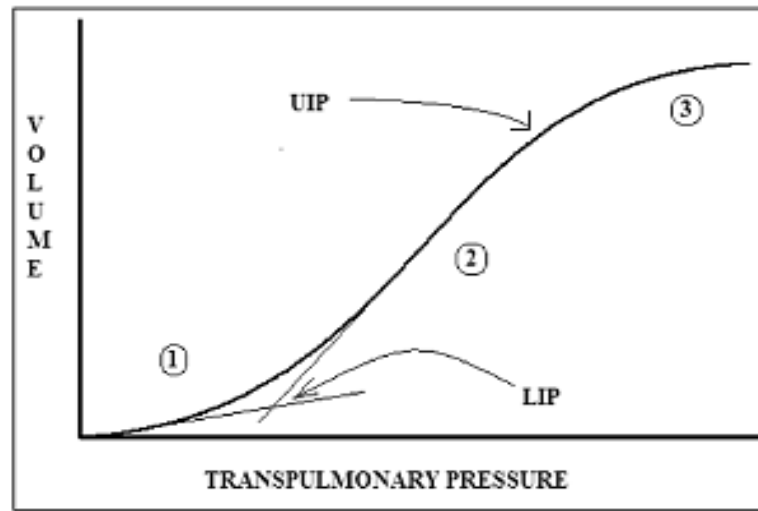
Basınç Kontrollü Ventilasyonda P-V Eğrisi ile Kompliansın Değerlendirilmesi

PEEP VE KOMPLIANSA ETKİSİ



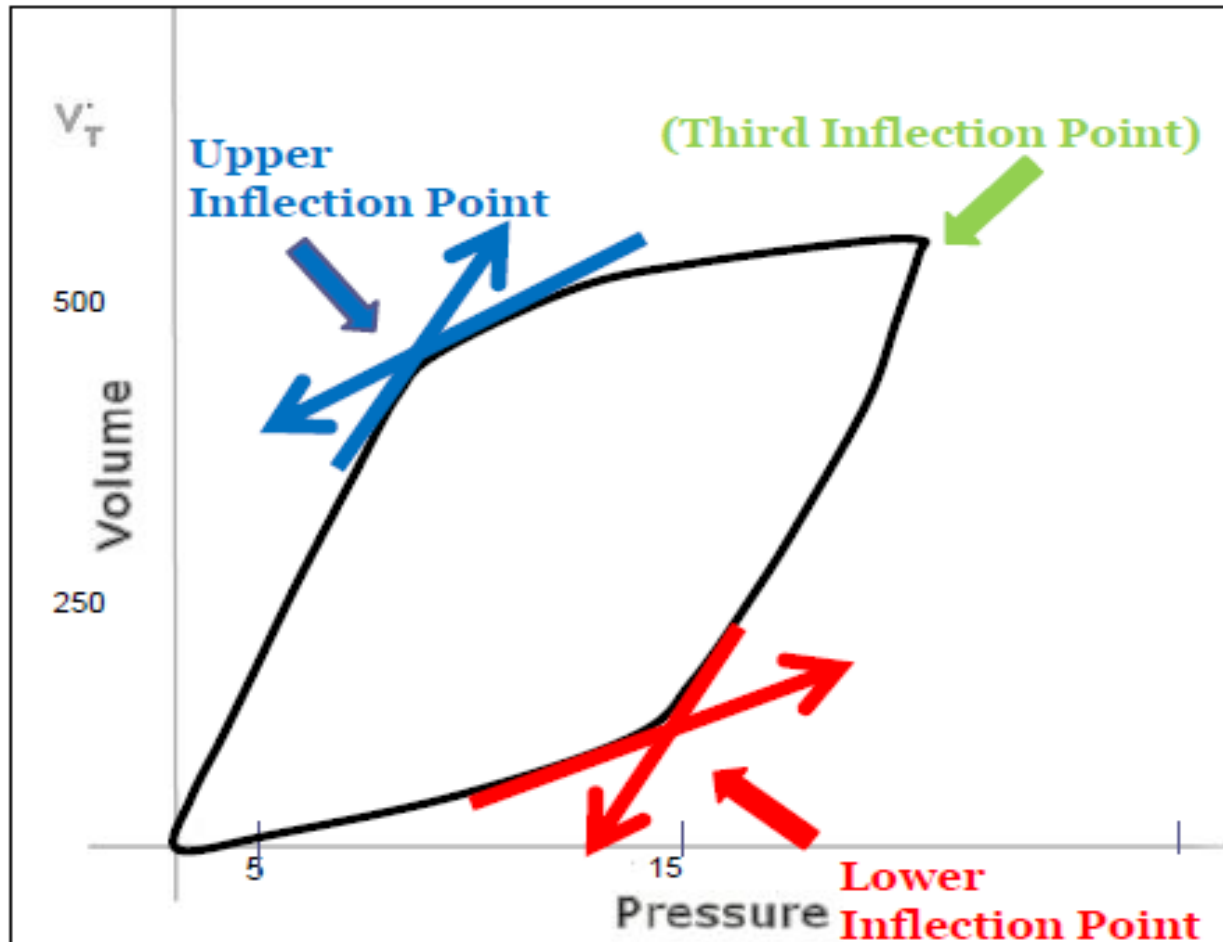
KOMPLIANS- PV EĞRİSİ

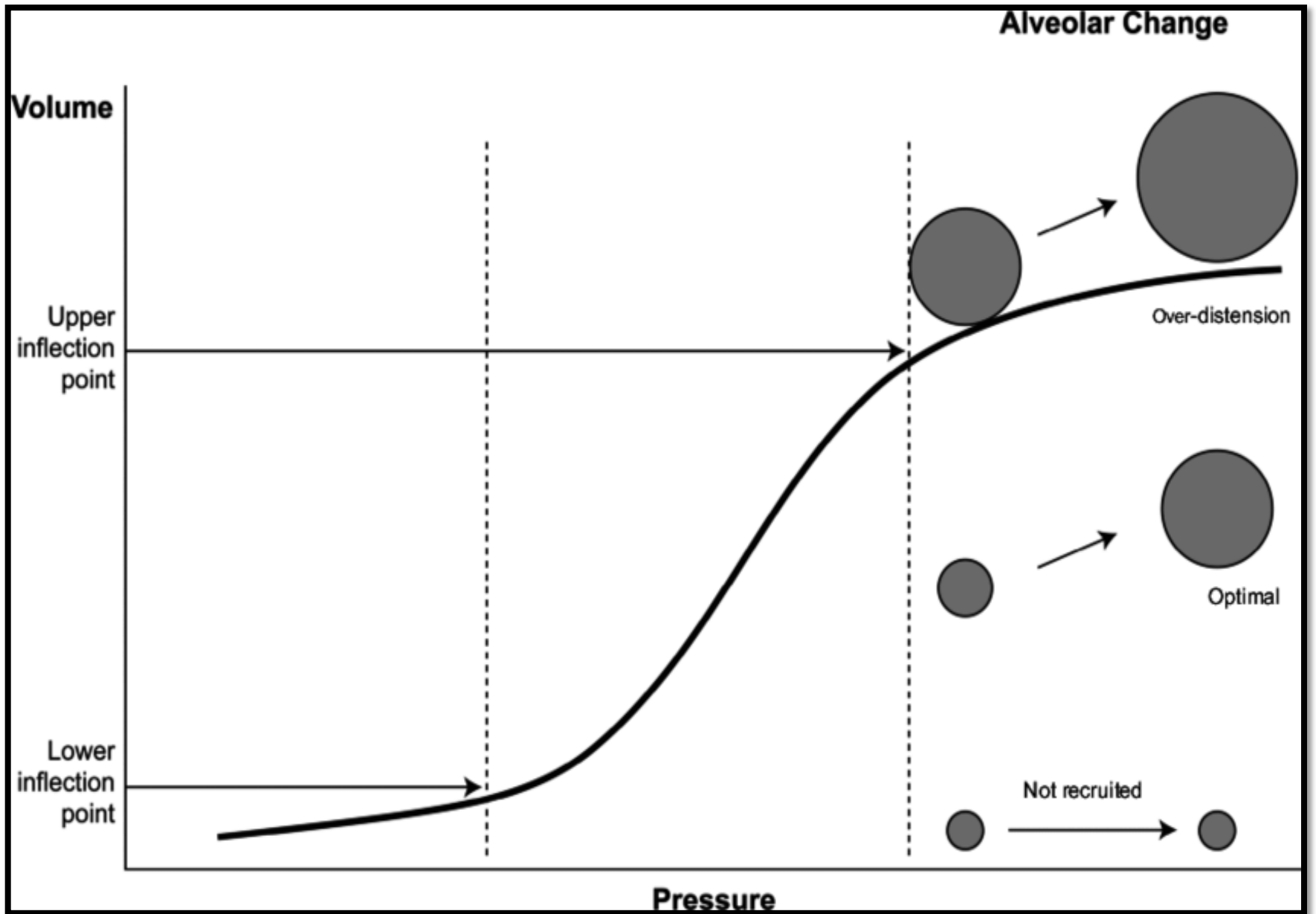
Figure 5



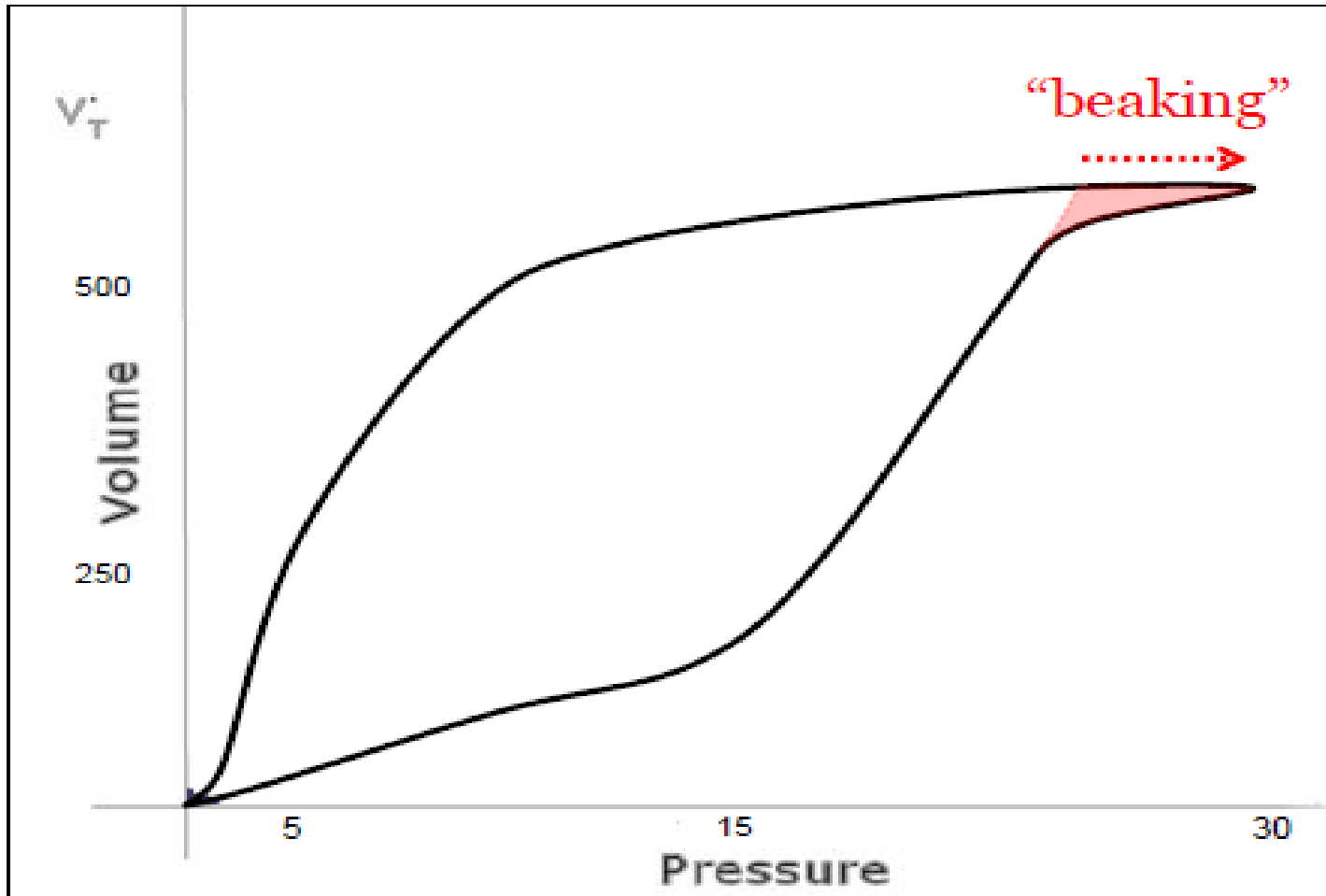
The inspiratory limb of the pressure–volume curve (dark line) divided into three sections. Section 1 (low compliance) and section 2 (high compliance) are separated by the lower inflection point (LIP). Section 2 (high compliance) and section 3 (low compliance) are separated by the upper inflection point (UIP). In this example, the LIP is marked at the point of crossing of the greatest slope in section 2 and the lowest slope of section 1. The UIP is marked at the point of 20% decrease from the greatest slope of section 2 (a calculated value).

ALT VE ÜST KIRILMA NOKTASI





AŞIRI DİSTANSİYON



KOMPLIANS

Table 1

Causes of decreased intrathoracic compliance

Causes of decreased measured chest wall compliance

Obesity
Ascites
Neuromuscular weakness (Guillain-Barre, steroid myopathy, etc.)
Flail chest (mediastinal removal)
Kyphoscoliosis
Fibrothorax
Pectus excavatum
Chest wall tumor
Paralysis
Scleroderma

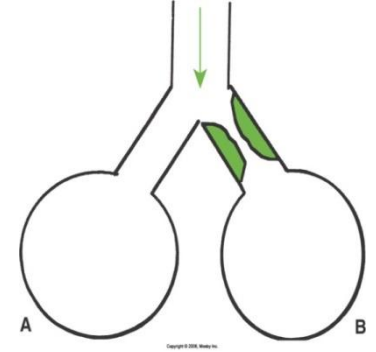
Causes of decreased measured lung compliance

Tension pneumothorax
Mainstem intubation
Dynamic hyperinflation
Pulmonary edema
Pulmonary fibrosis
Acute respiratory distress syndrome
Langerhans cell histiocytosis
Hypersensitivity pneumonitis
Connective tissue disorders
Sarcoidosis
Cryptogenic organizing pneumonitis
Lymphangitic spread of tumor

Shown are the causes of decreased intrathoracic compliance, partitioned into causes of decreased measured chest wall compliance and causes of decreased measured lung compliance.

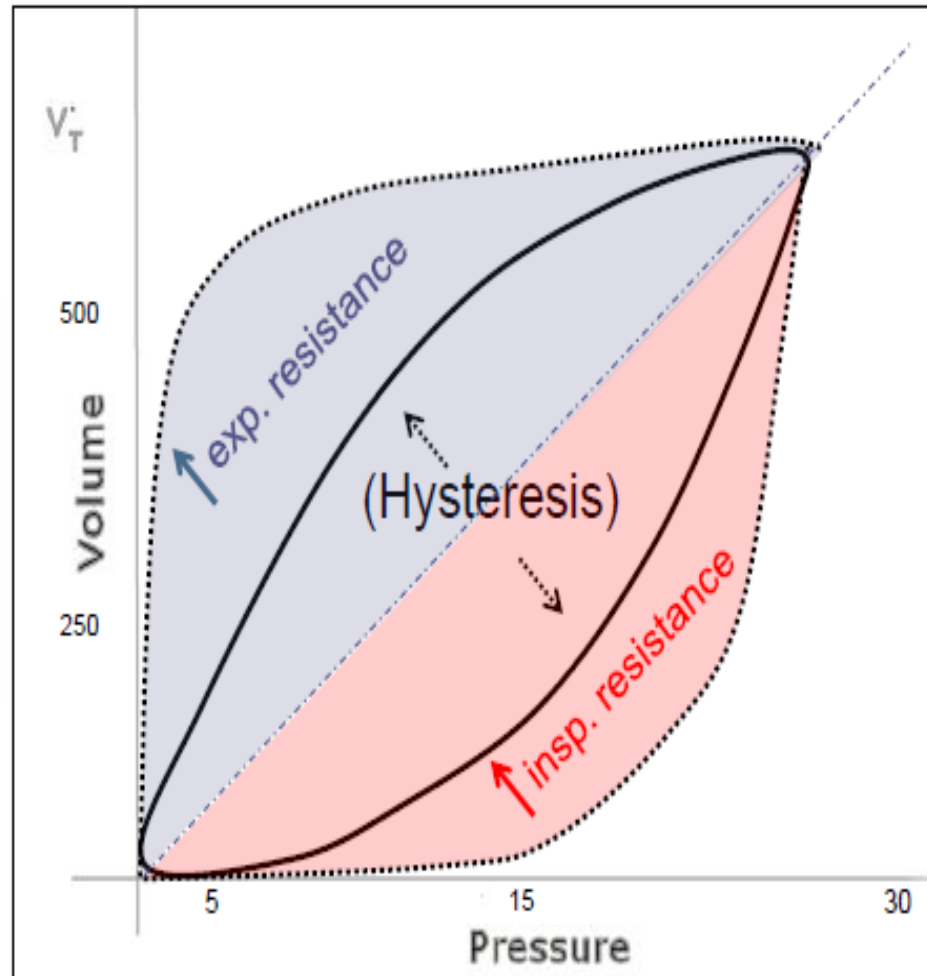
SOLUNUM MEKANİKLERİ

- **Rezistans: «Akıma karşı direnç»**
 - İletici hava yolları sorumludur
 - Akım Hızı: Tidal Volüm / İspirasyon süresi
 - **Rezistans: $P_{peak} - P_{plateau} / \text{Akım Hızı}$**
 - **Raw (cmH2O/L/sn):**
 - Entübe olmayanlarda: 0.6-2.4 cmH2O/L/sn
 - Entübelerde ≥ 6 cmH2O/L/sn
 - **Endotrakeal tüp rezistans artışında önemli!!**
 - Tüp ne kadar küçük olursa, rezistans o kadar fazla olur
 - Hava yolu hastalıkları rezistansı artırır



PV Eğrisi

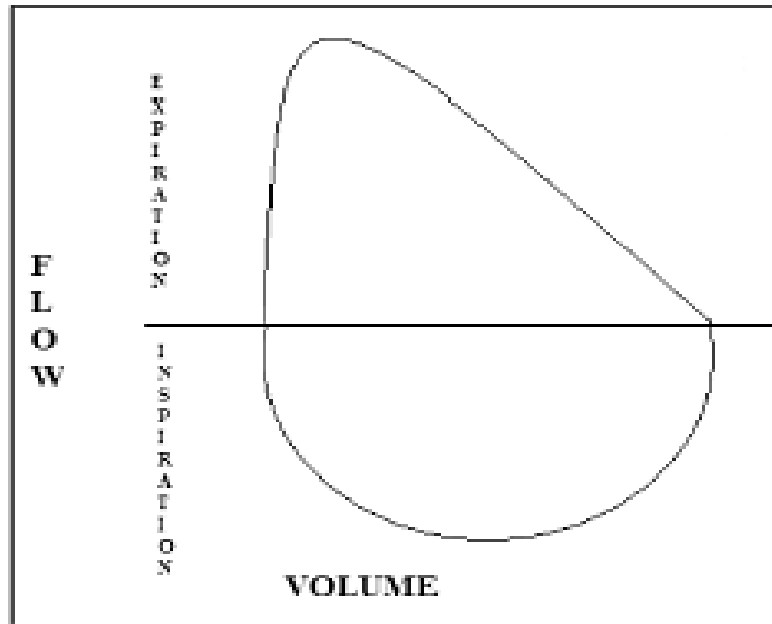
Increased expiratory resistance:
secretions,
bronchospasms,
etc.



Increased inspiratory resistance:
kinked ET tube,
patient biting
tube

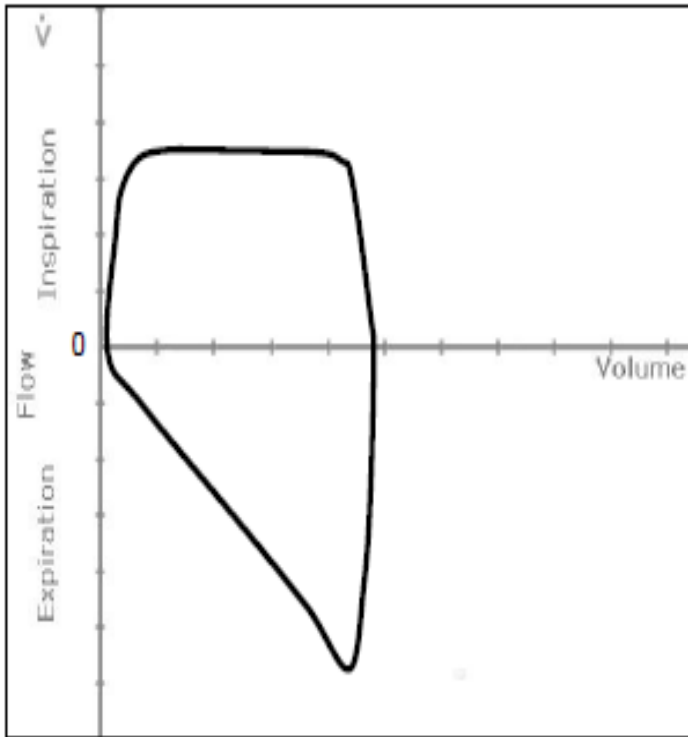
SOLUNUM MEKANİKLERİ

AKIM VOLÜM EĞRİSİ

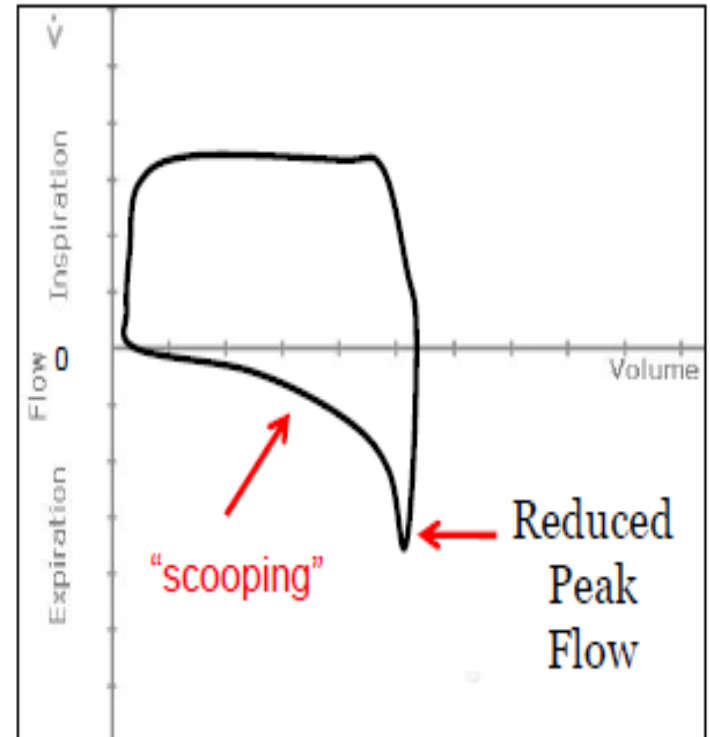


Flow–volume loop. A flow–volume loop is shown, with exhalation above the horizontal axis and inspiration below.

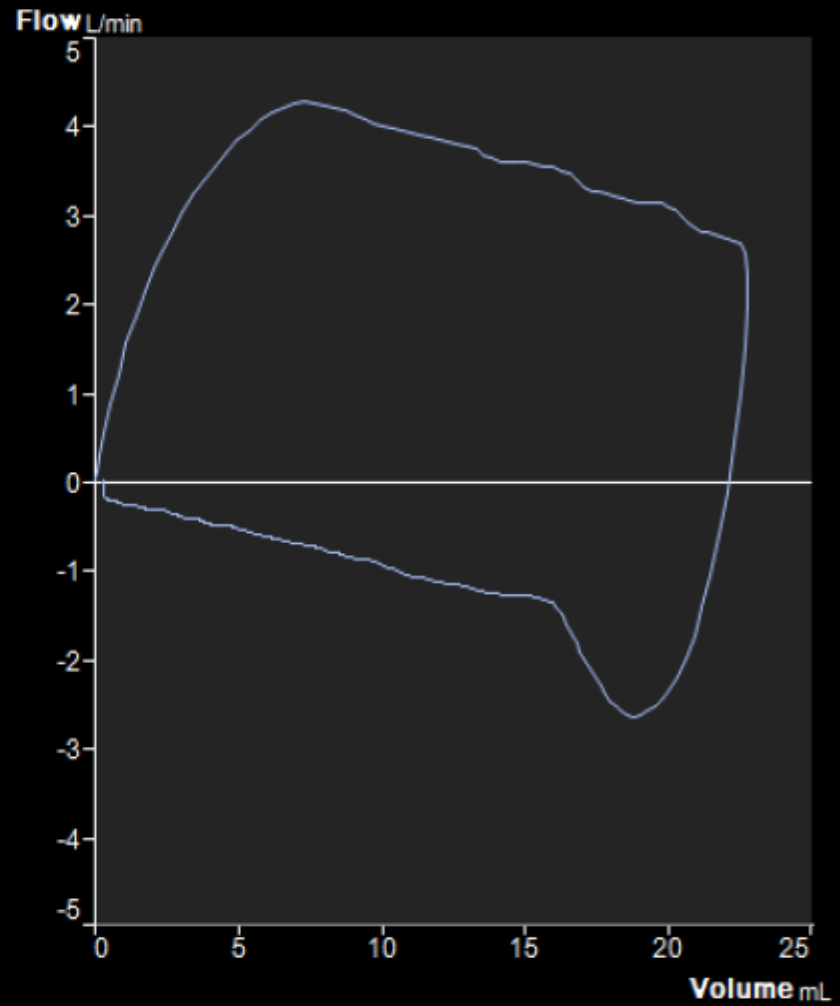
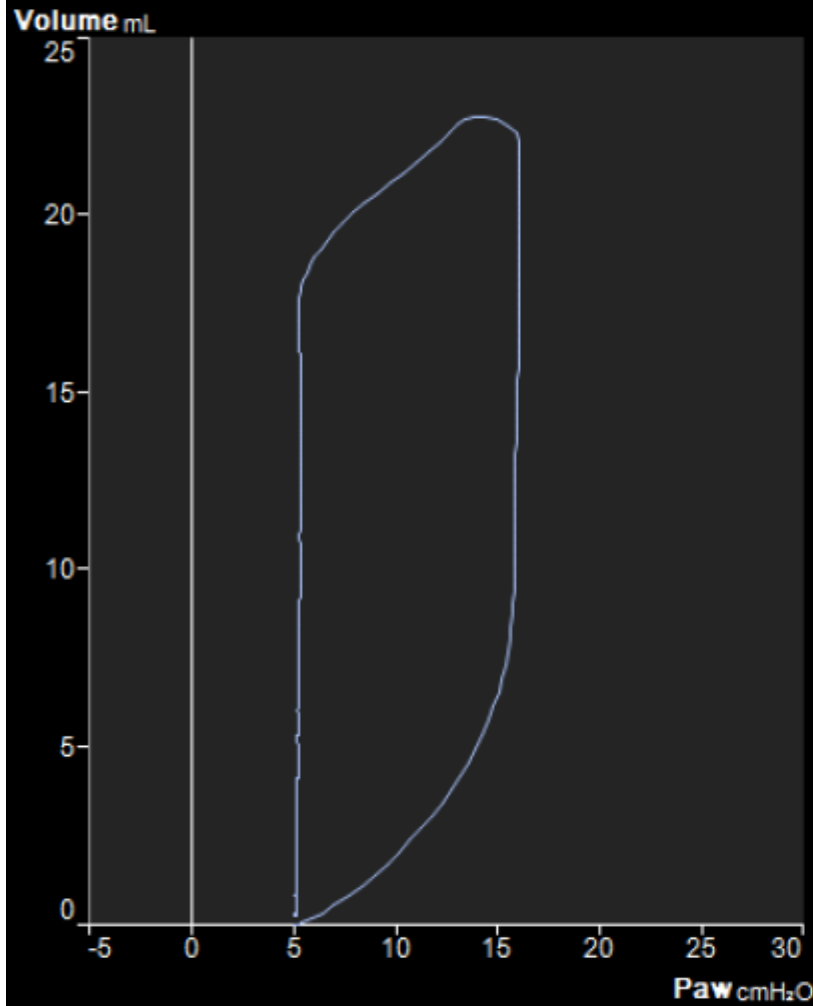
HAVAYOLU OBSTRÜKSİYONU



“normal
vent graphic
view”



BRONKOKONSTRİKSİYON

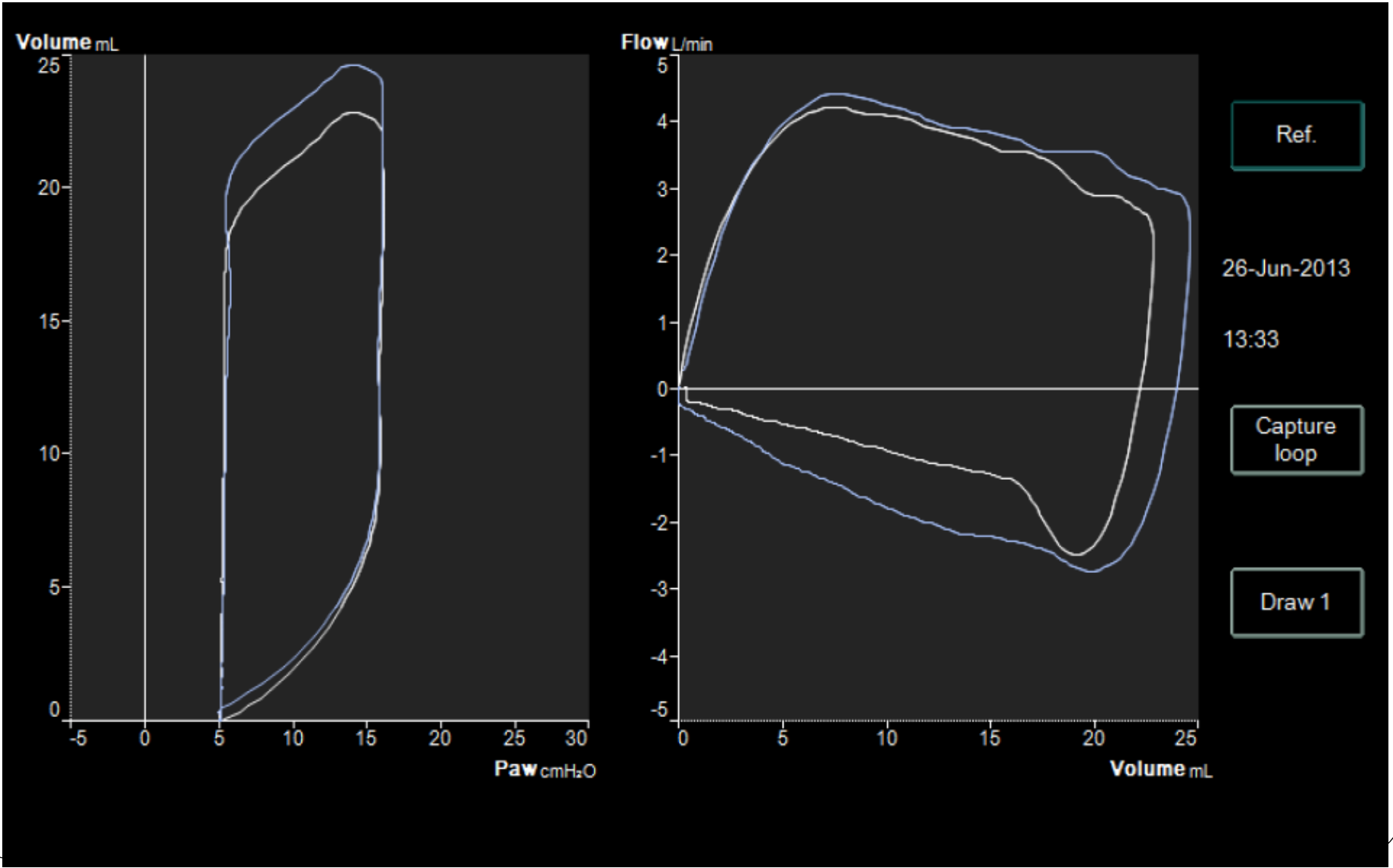


Ref.

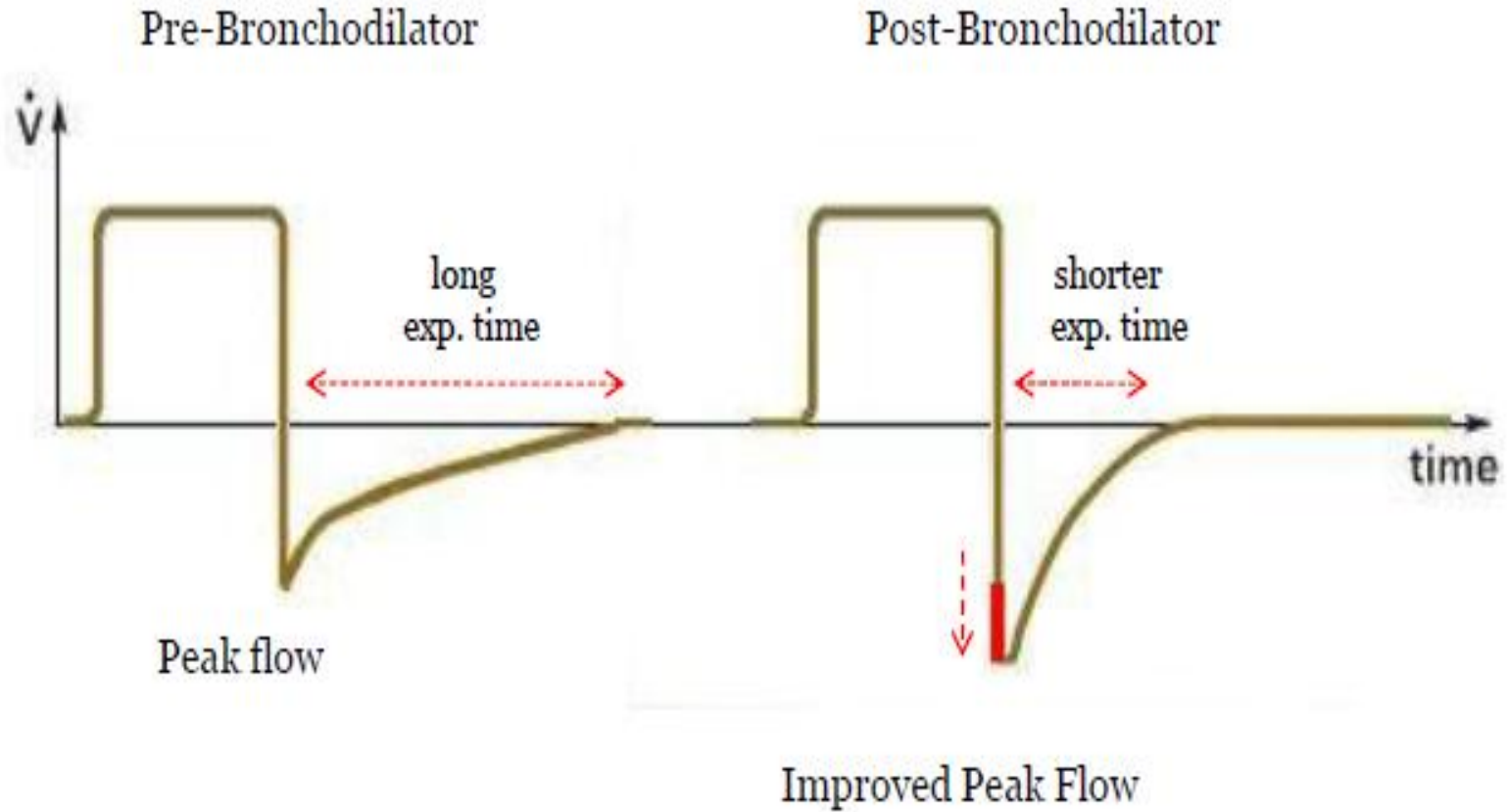
Capture loop

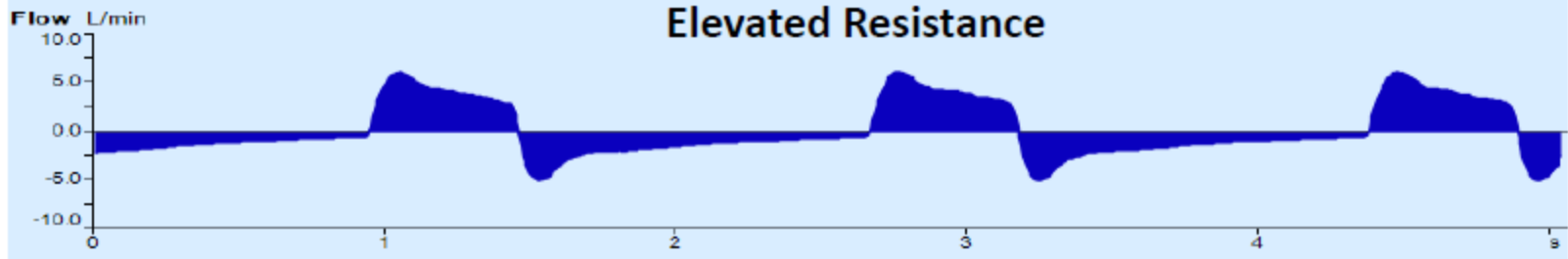
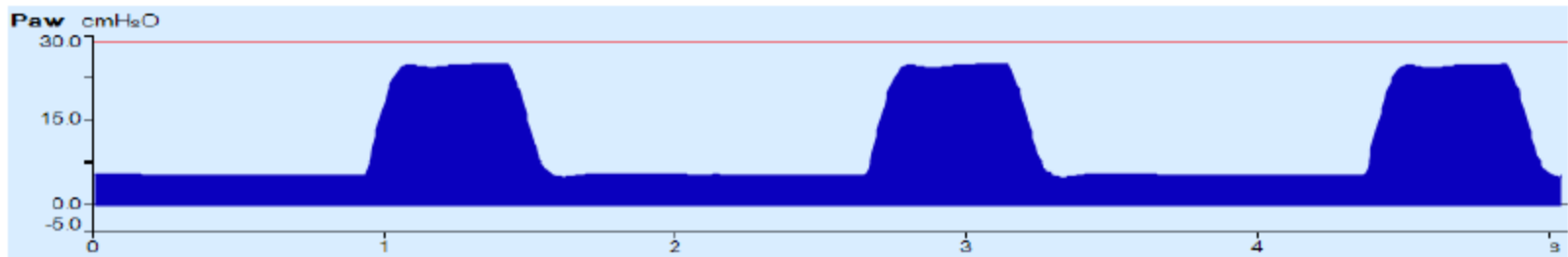
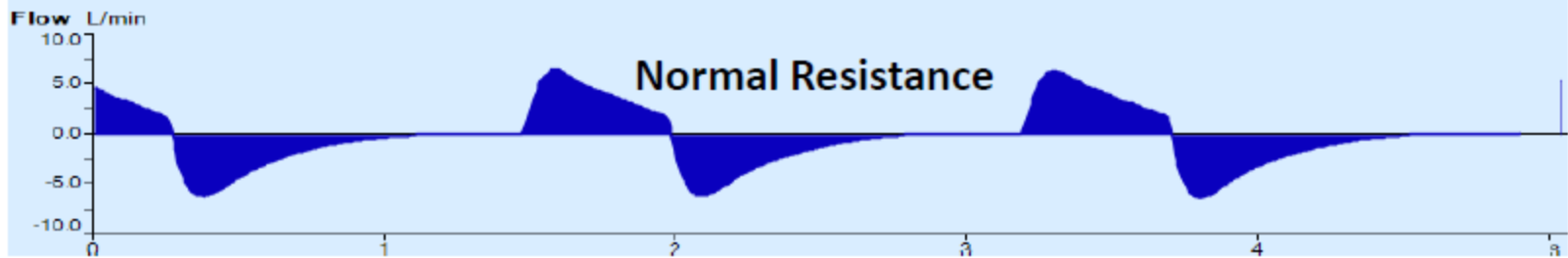
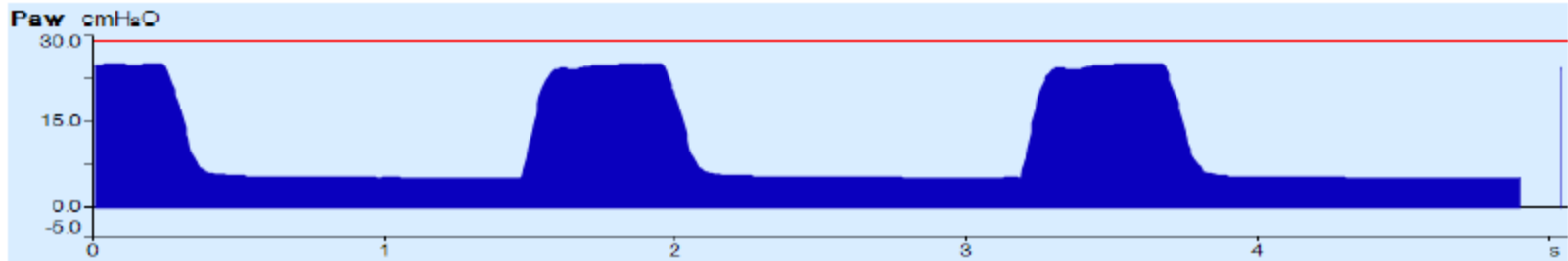
Draw 1

BRONKODİLATÖR TEDAVİ SONRASI



BRONKODİLATÖR CEVABI

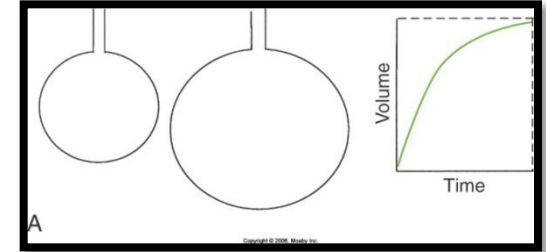




SOLUNUM MEKANİKLERİ

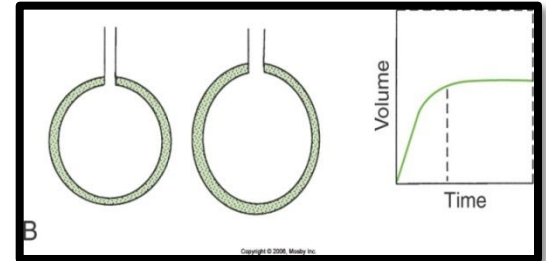
Zaman Sabiti: Komplians x Rezistans

A: Normal AC



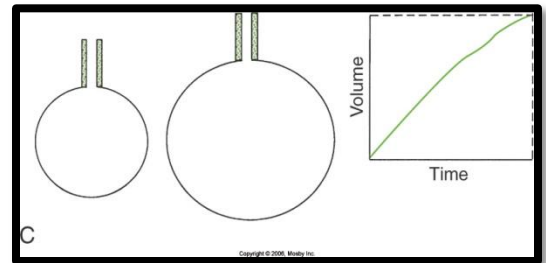
B: Düşük komplians;

alveoller hızlıca dolar ama daha az hava girer
(Kısa zaman sabiti; örn ARDS)



C: Artmış rezistans;

alveoller yavaş dolar, daha yavaş boşalır.
(Uzun zaman sabiti; örn KOAH)



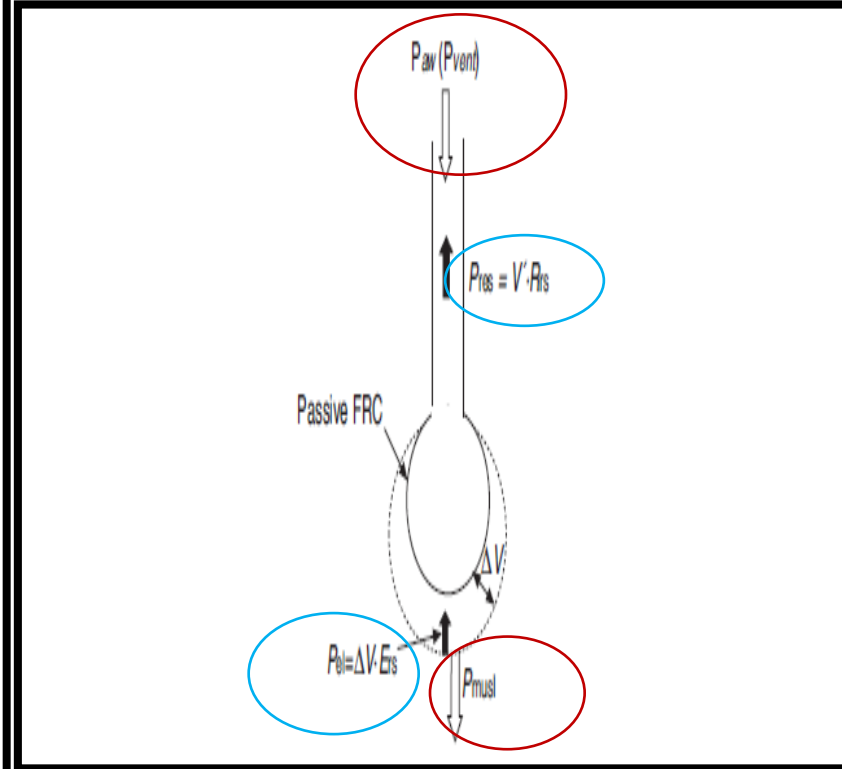
SOLUNUM MEKANİKLERİ

Pozitif Basıncılı Ventilasyonda Gaz Akımı Temel Denklemi

= (Ventilatör tarafından oluşturulan pozitif basınç)+ (inspiratuar kaslar tarafından oluşturulan negatif plevral basınç)

= P elastans + P resistive

= (Elastans x Volüm)+(Rezistans x Akım)



$$P_{tot} (t) = P_{mus}(t) + P_{aw}(t) = V'(t) \cdot R_{rs} + V_T(t) \cdot E_{rs} + PEEP_i$$

**SOLUNUM MEKANİKLERİNİN
YATAK BAŞINDA
DEĞERLENDİRİLMESİ**

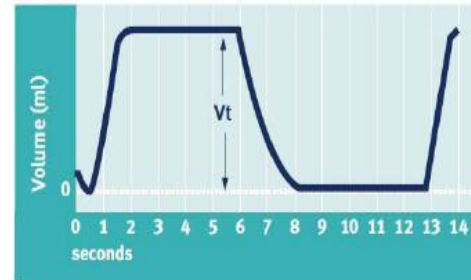
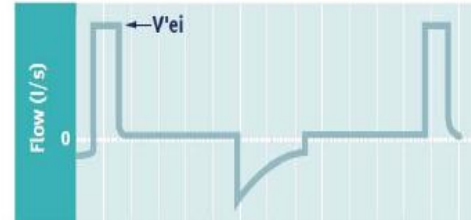
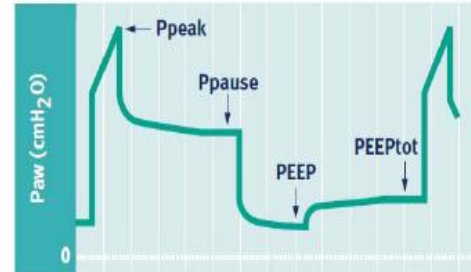
SOLUNUM MEKANİKLERİ

● Peak Inspiratuar Basınç (PIP):

- Inspiratuar fazdaki en yüksek basınç
- Belirleyen faktörler
 - AC-Göğüs duvarı kompliansı
 - Havayolu rezistansı
 - Verilen tidal volüm
 - Inspiratuar akım hızı
 - End ekspiratuar basınç(PEEP)
 - Solunum iş yükü (WOB)

● Inspiratuar pause:

- Amaç: AC'de havanın dağılımını düzeltmek
- Optimum V/Q uyumunu sağlamak
- VD/VT oranını azaltmak

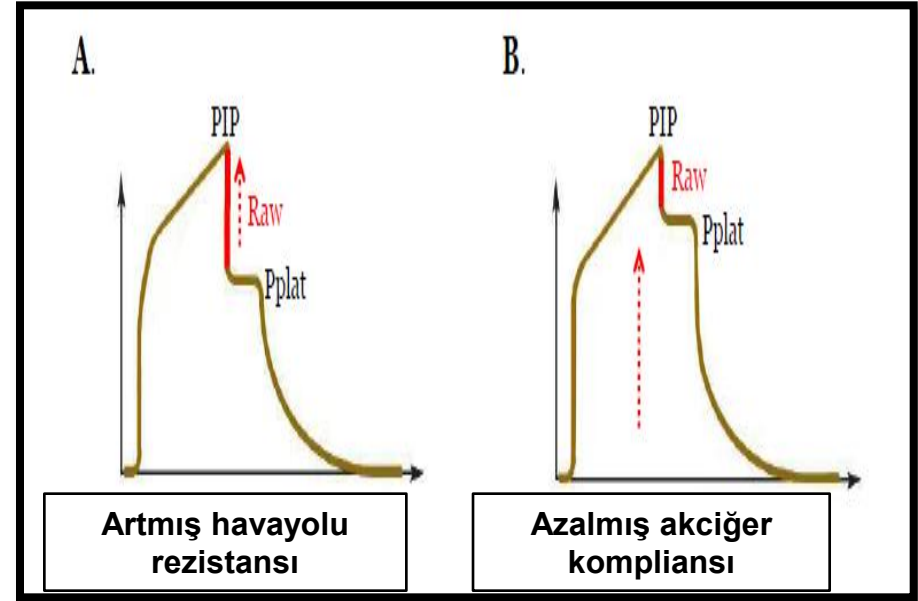
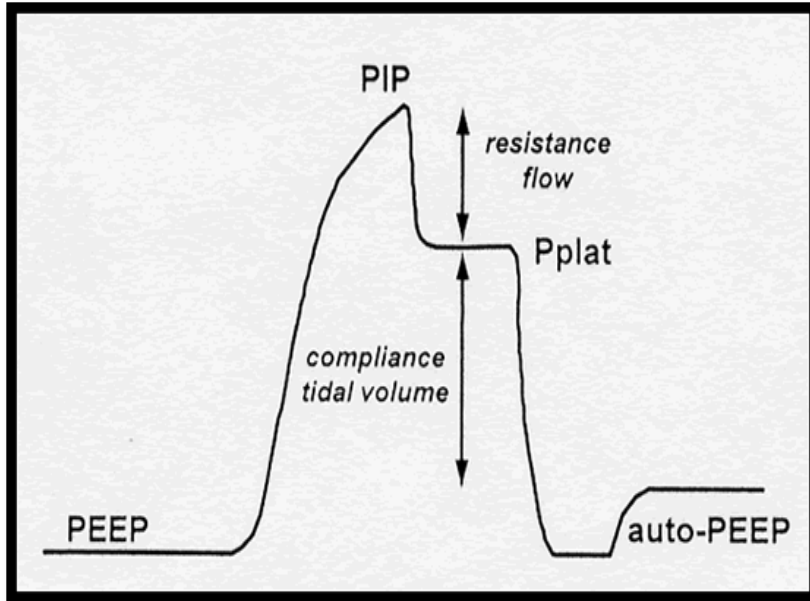


In ventilated adults with normal airway resistance, $R_{i,max}$ is usually 5-8 cmH2O/l/s (including the effect of an unobstructed endotracheal tube of appropriate size). The clinical interpretation of measurements of respiratory system compliance is easier when referred to the ideal body weight (normal value: 1-1.2 ml/cmH2O/kg).

- Ppeak = peak airway pressure
- Ppause = static end-inspiratory pressure
- PEEP = positive end-expiratory pressure
- PEEPtot = total intrapulmonary PEEP
- V'ei = end-inspiratory flow
- Vt = tidal volume
- $R_{i,max} = \frac{P_{peak} - P_{pause}}{V'_{ei}}$
- $C_{qs} = \frac{V_t}{P_{pause} - PEEP_{tot}}$
- RC = $R_{i,max} \cdot C_{qs}$
- PEEPi = PEEPtot - PEEP

Frozen curves during passive VCV with constant inspiratory flow and double hold manoeuvre, for manual measurement of passive respiratory system mechanics

SOLUNUM MEKANİKLERİ



$$C_{strs} = \frac{V_T}{P_{plat} - PEEP_{total}} \quad R_{aw} = \frac{PIP - P_{plat}}{\dot{V}_i}$$

**PPlato ≤ 30cmH2O
tutulmalı**

Driving Pressure-Plato Pressure

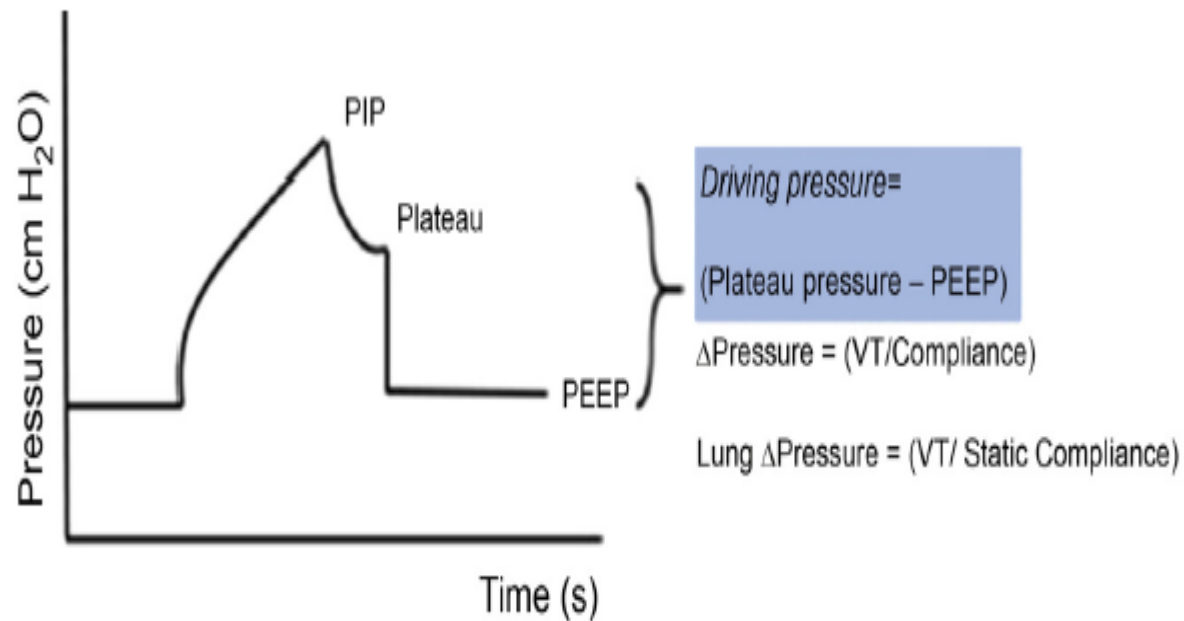


Fig. 21. DP is the difference between P_{plat} and PEEP, and is a correlate of the ratio between VT and the compliance of the respiratory system.

Driving Pressure-Plato Pressure

- **ΔP (Driving Pressure);**
 - Tidal volumun akciğerde ne kadar mekanik bozulma (dinamik strain) yarattığını tahmin eder,
- **Plato basıncı (P_{plato});**
 - Akciğere uygulanan basıncı (akciğer stresi) yansıtır.
- Her ikisi de barotravma riskini ölçer.

Stres indeks

- Sabit akımlı volüm kontrol ventilasyon sırasında basınç zaman eğrisinin şekli değerlendirilerek elde edilir

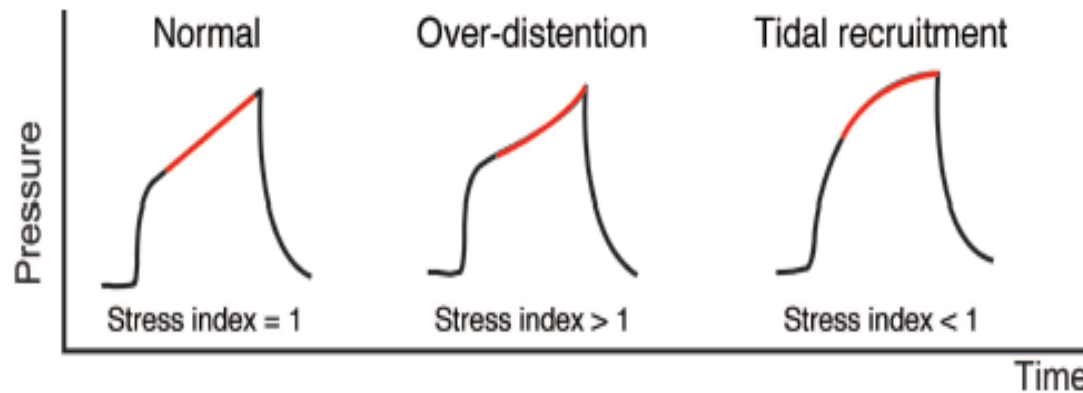


Fig. 10. Normal stress index, stress index with over-distention, and stress index with tidal recruitment.

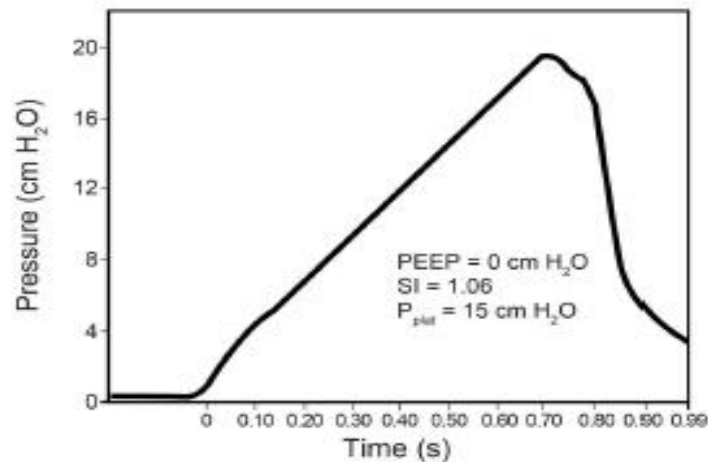
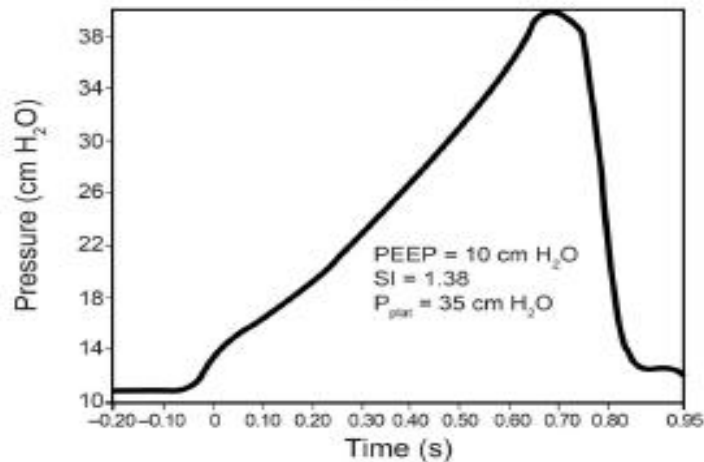
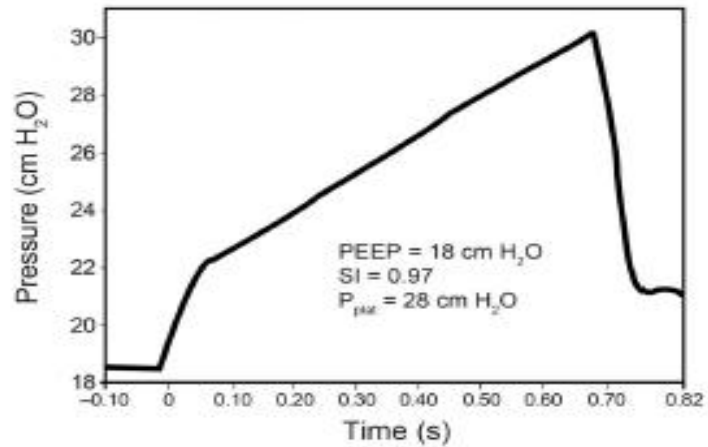
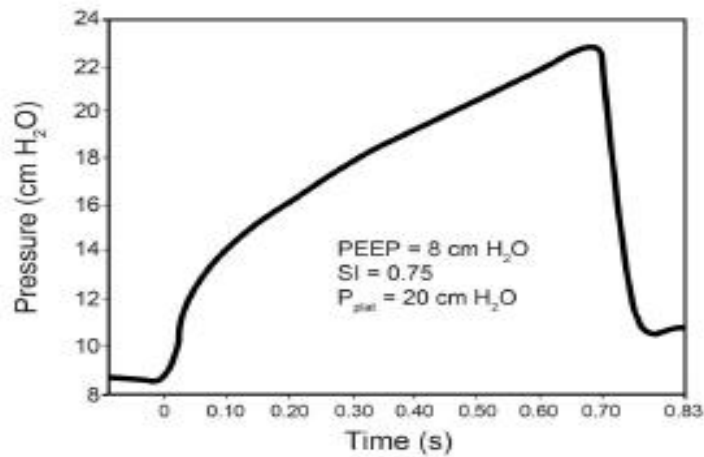
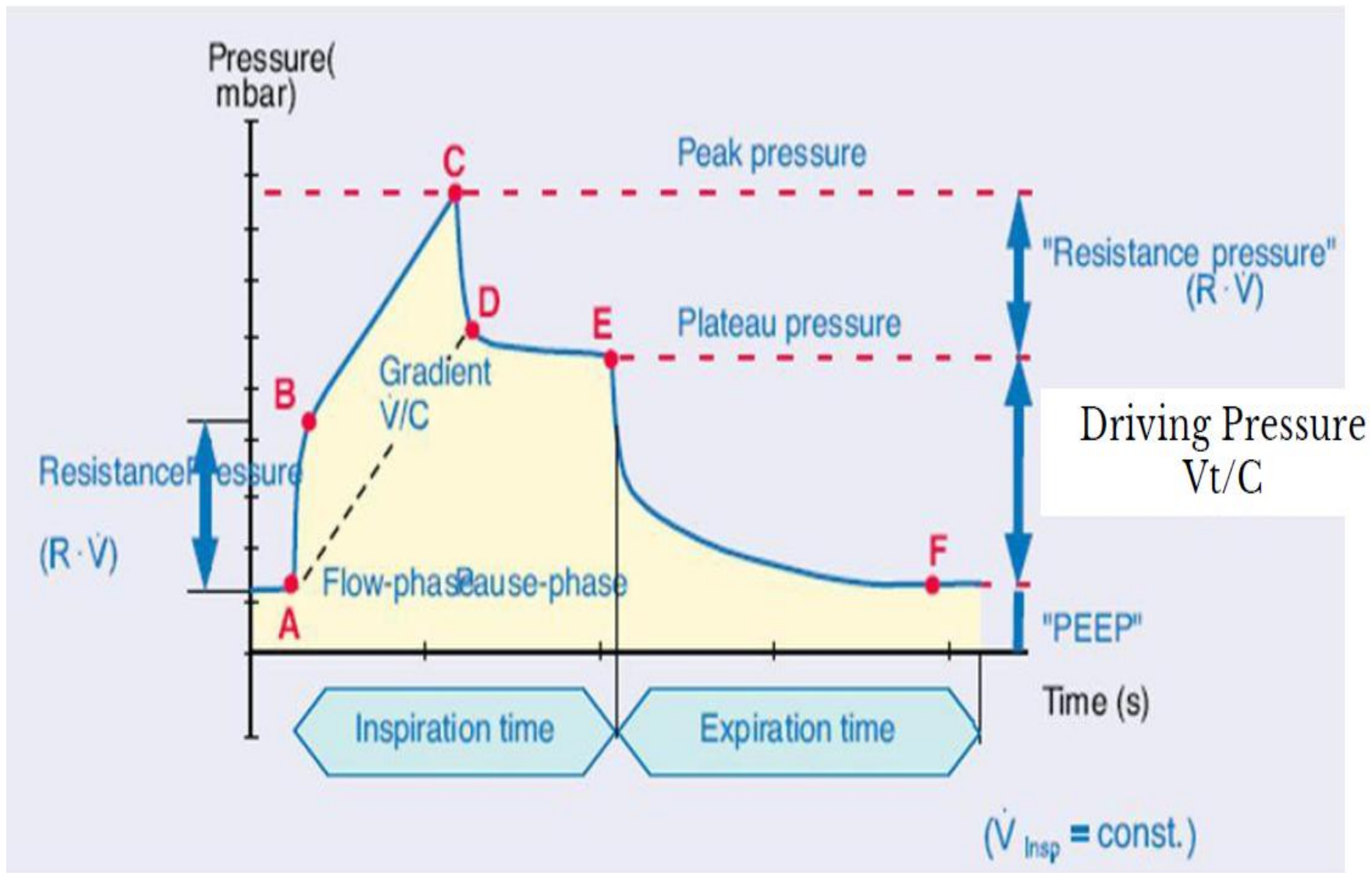
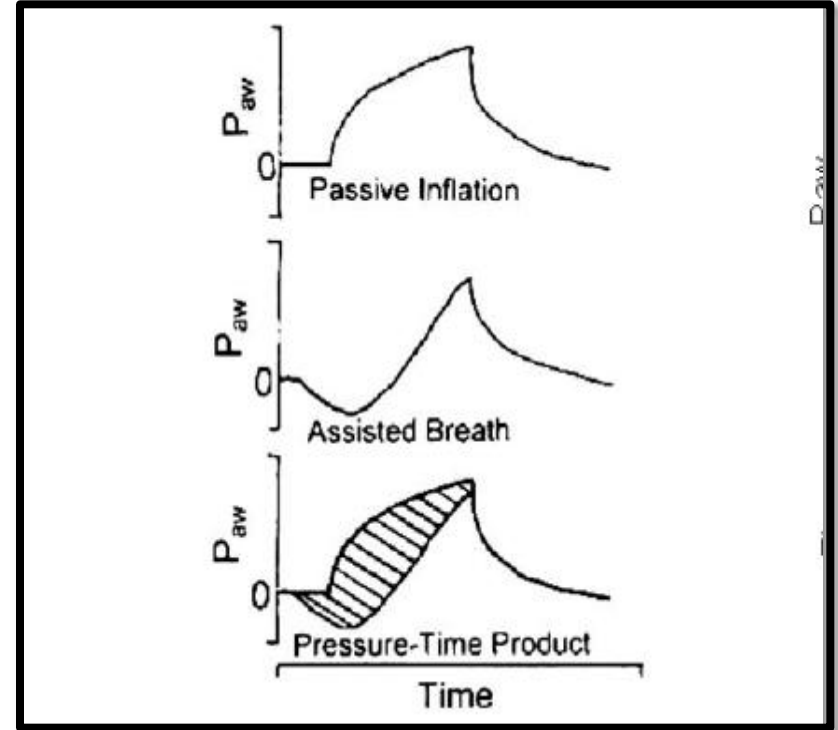
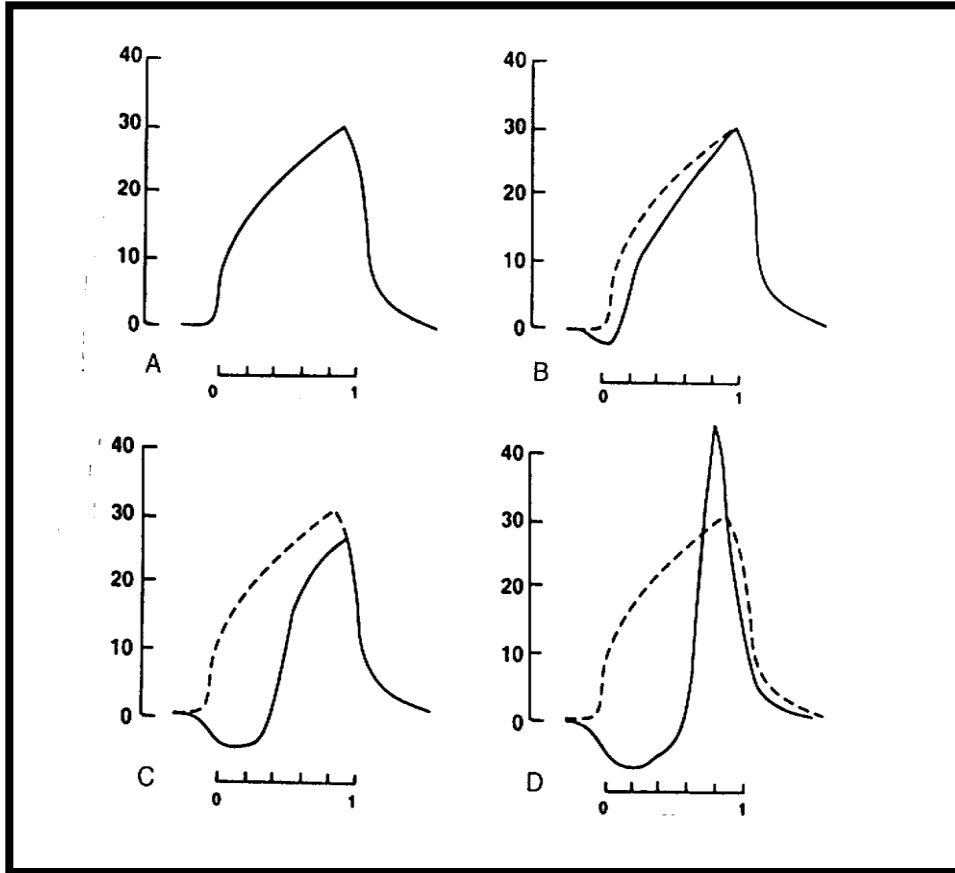


Fig. 11. Top: Stress index (SI) in a patient early in the course of ARDS. In this case, the stress index improved as PEEP was increased. Bottom: Stress index in a patient late in the course of ARDS. In this case, the stress index improved as PEEP was decreased. P_{plateau} – plateau pressure. From Reference 31.

Pressure – time curve (volume – oriented mode)



AKIM HIZI YETERLİ Mİ?



Kaynak: Pilbeam SP. Basic terms and concepts of mechanical ventilation.,in Mechanical Ventilation:Physiological and Clinical Applications ed 4, St Louis 2006, Mosby

Solunum Mekaniklerinin Yatak Başında Değerlendirilmesi-Expiratory Hold

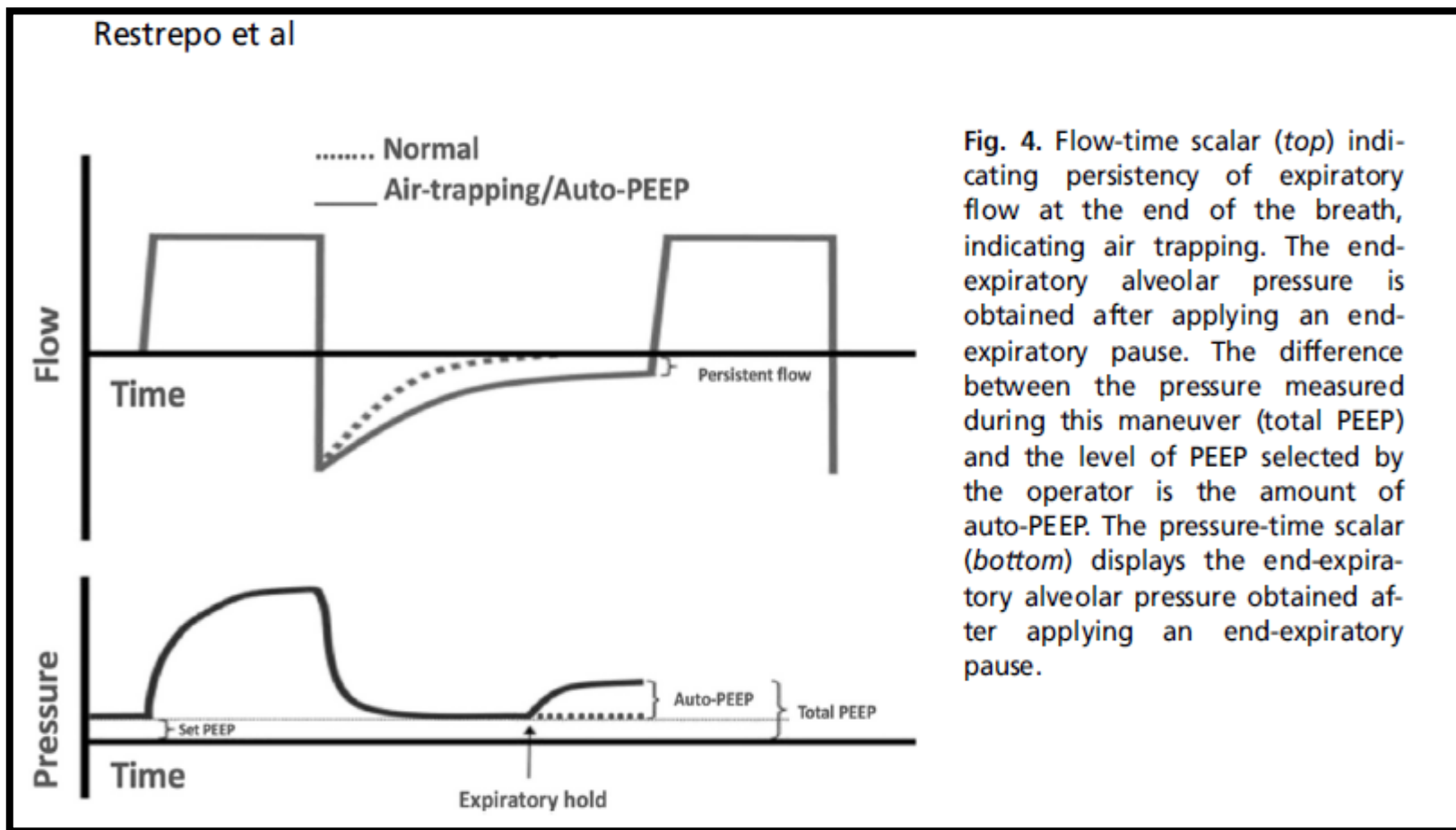
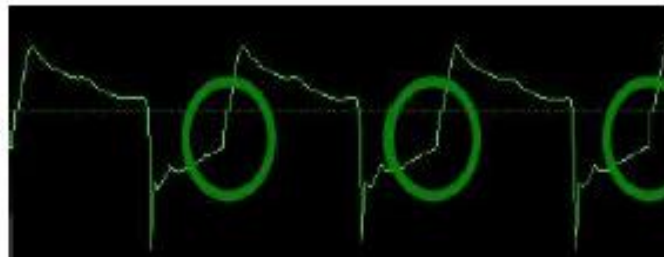
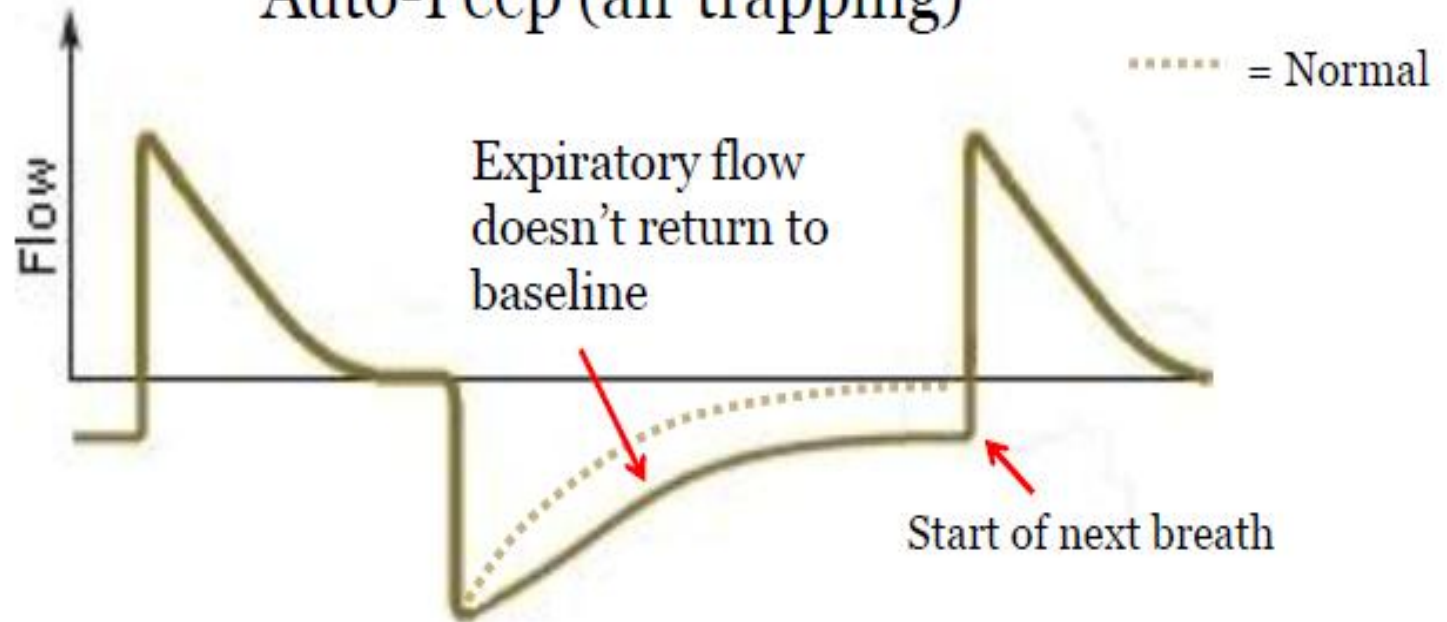


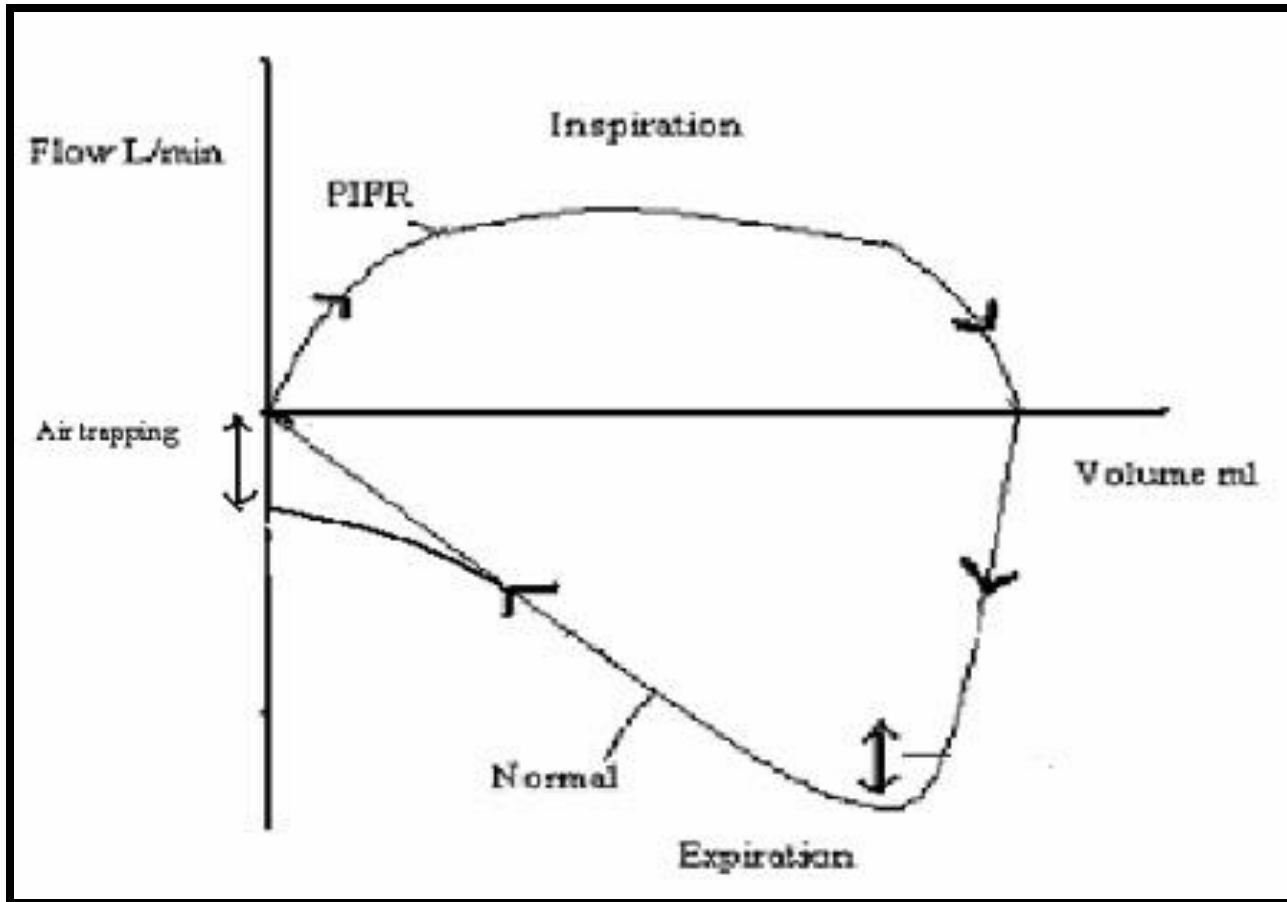
Fig. 4. Flow-time scalar (*top*) indicating persistency of expiratory flow at the end of the breath, indicating air trapping. The end-expiratory alveolar pressure is obtained after applying an end-expiratory pause. The difference between the pressure measured during this maneuver (total PEEP) and the level of PEEP selected by the operator is the amount of auto-PEEP. The pressure-time scalar (*bottom*) displays the end-expiratory alveolar pressure obtained after applying an end-expiratory pause.

HAVA HAPSI-OTO PEEP

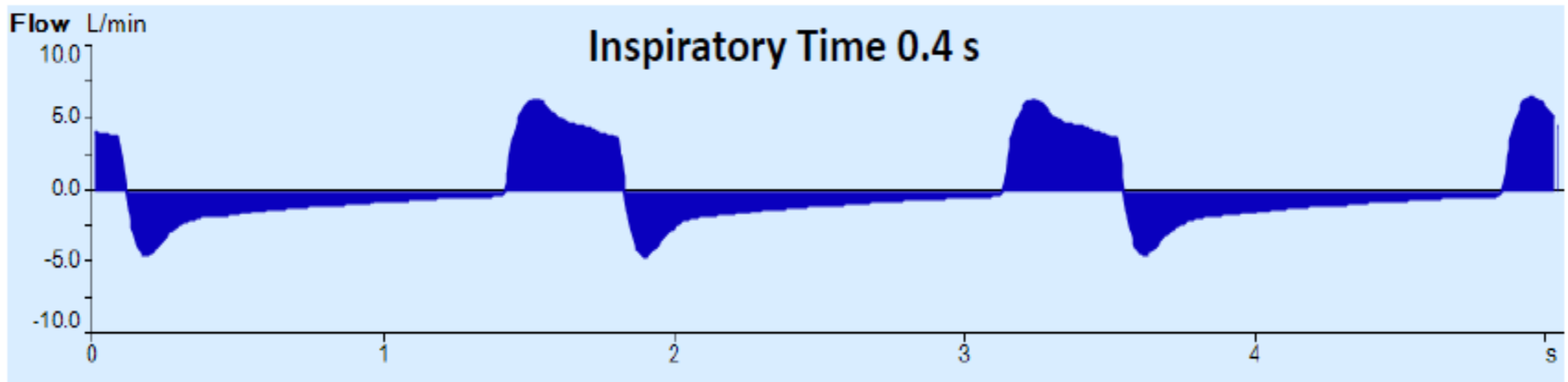
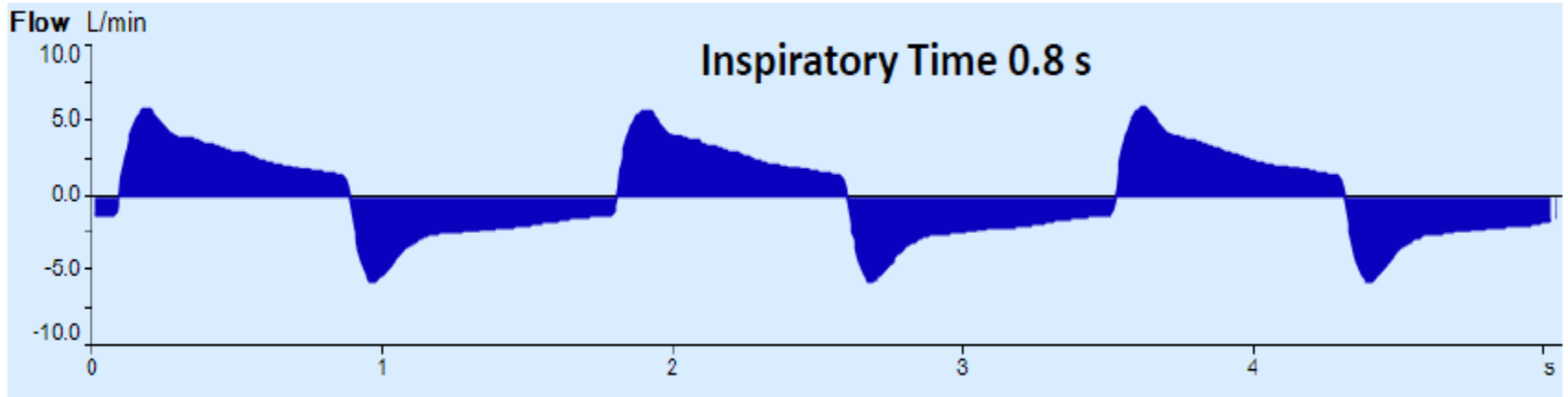
Auto-Peep (air trapping)



HAVA HAPSI-OTO PEEP



HAVA HAPSI-OTO PEEP

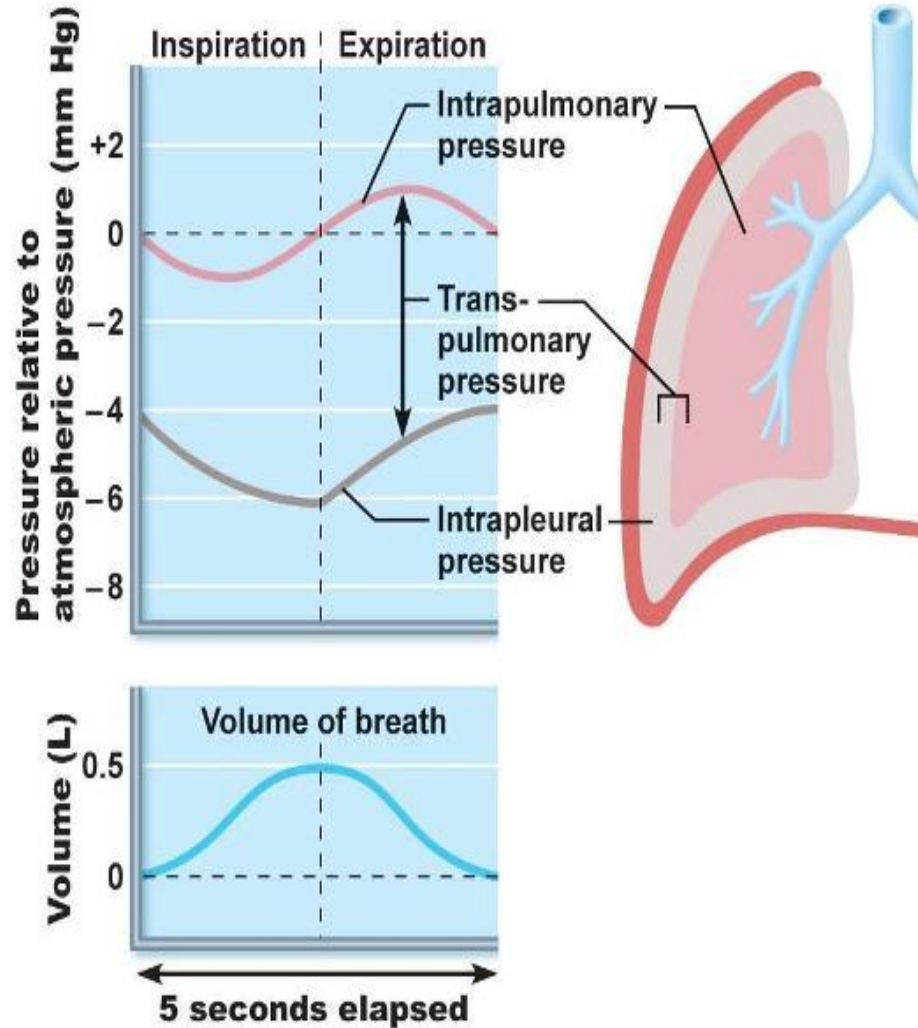


**ÖZAFAGEAL (PLEVRAL)
VE GASTRİK (ABDOMİNAL)
BASINÇLAR**

Intrapulmonary pressure. Pressure inside lung decreases as lung volume increases during inspiration; pressure increases during expiration.

Intrapleural pressure. Pleural cavity pressure becomes more negative as chest wall expands during inspiration. Returns to initial value as chest wall recoils.

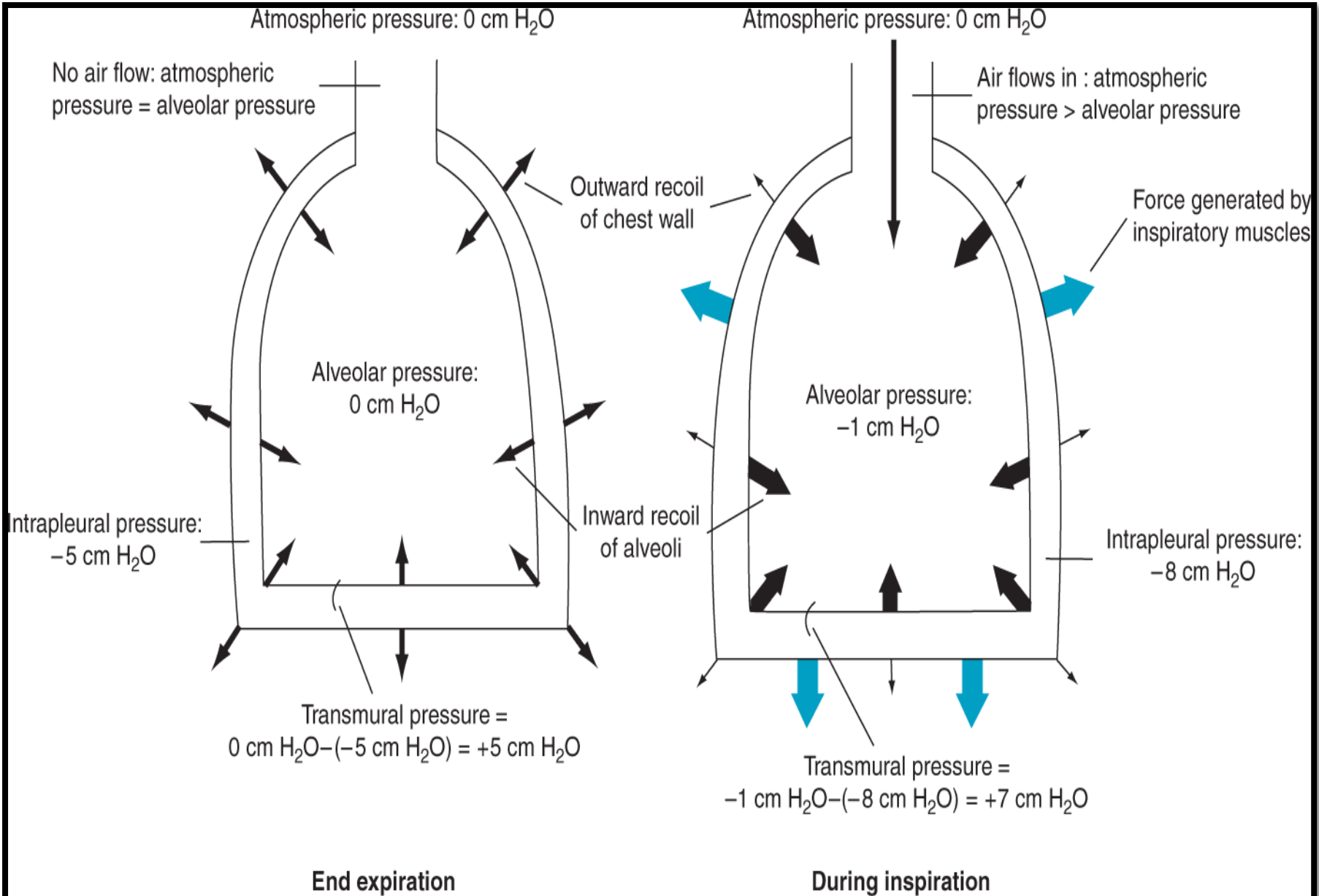
Volume of breath. During each breath, the pressure gradients move 0.5 liter of air into and out of the lungs.



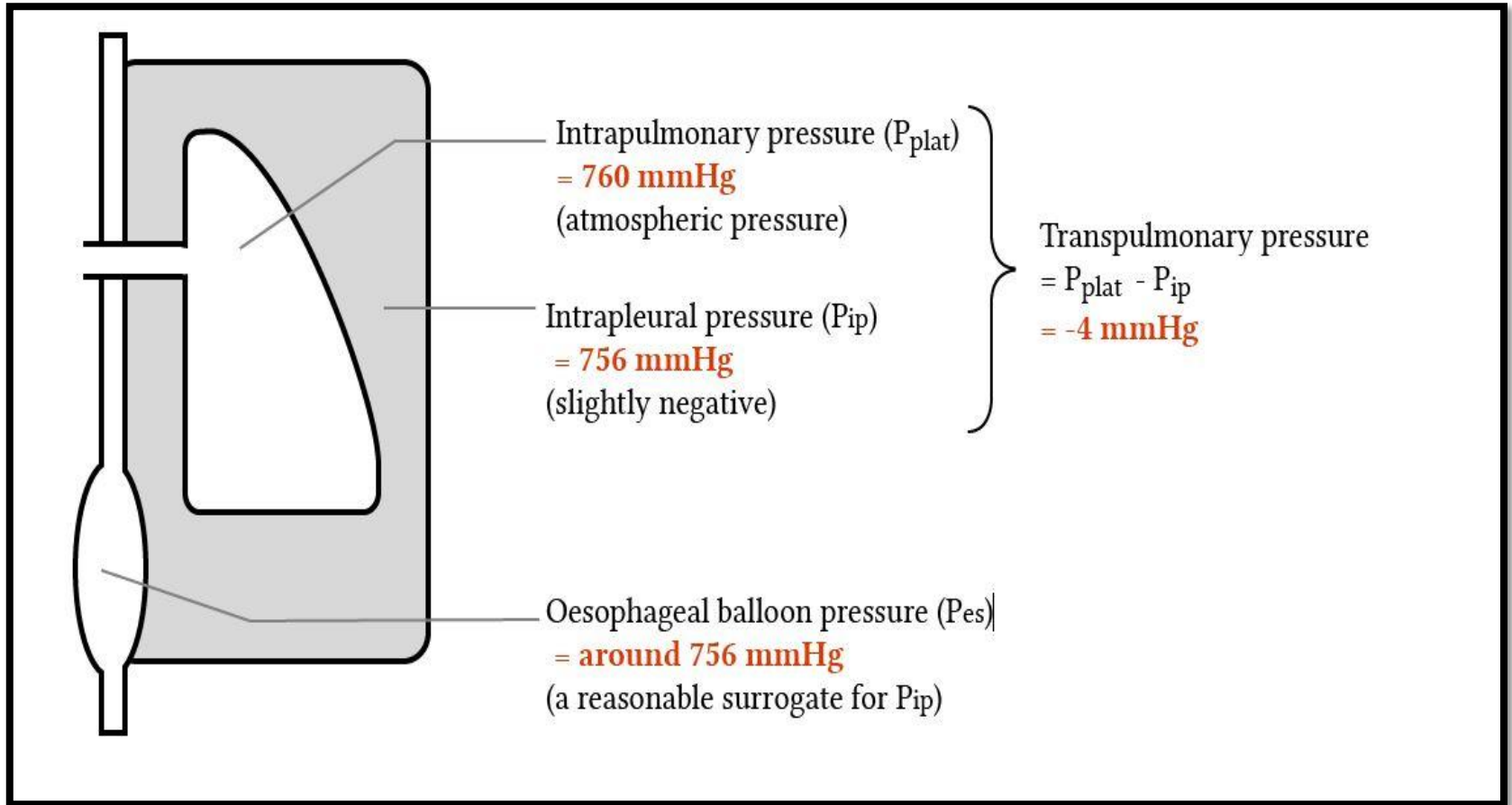
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Transpulmoner P(P_L): P_A-P_{pl}

alveolar havalanmadan sorumludur.



TRANSPULMONER BASINÇ



ÖZAFAGEAL (PLEVRAL) VE GASTRİK (ABDOMİNAL) BASINÇLAR

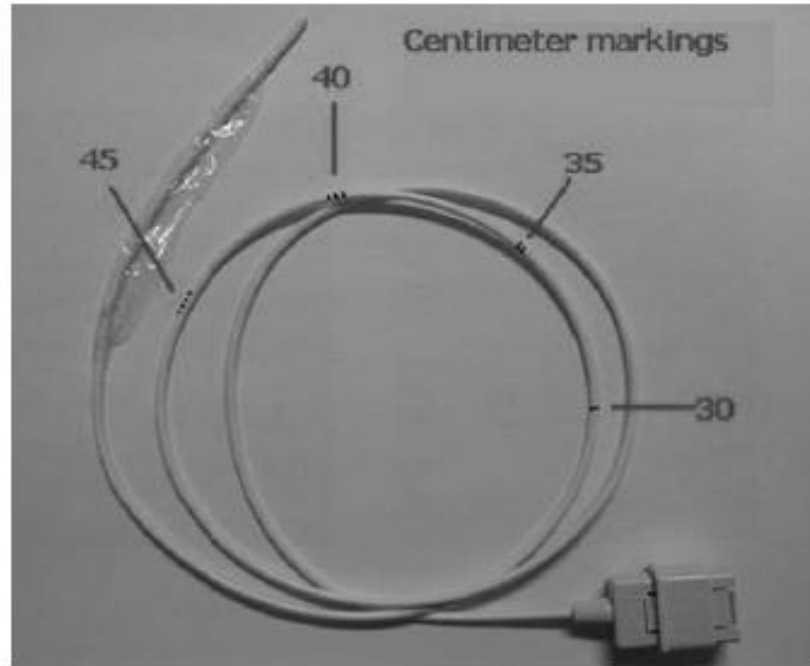


Fig. 1. Picture of an esophageal manometer demonstrating the size and position of the balloon, as well as the depth markings in centimeters.

ÖZAFAGEAL (PLEVRAL) VE GASTRİK (ABDOMİNAL) BASINÇLAR

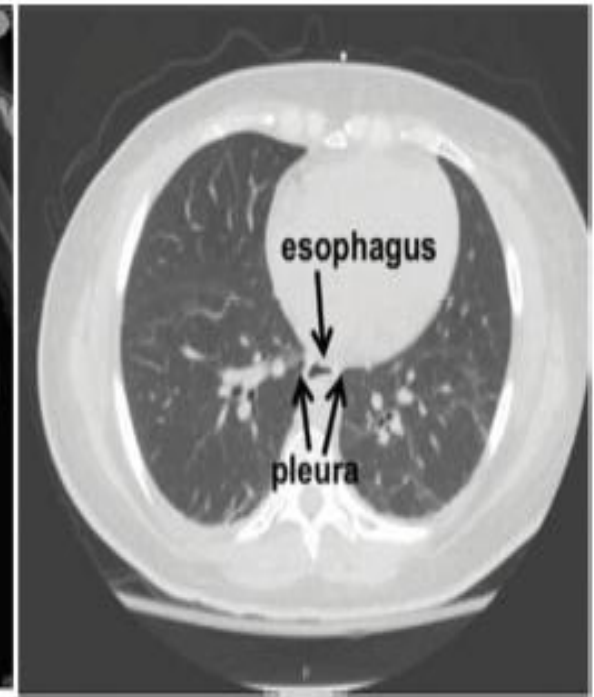
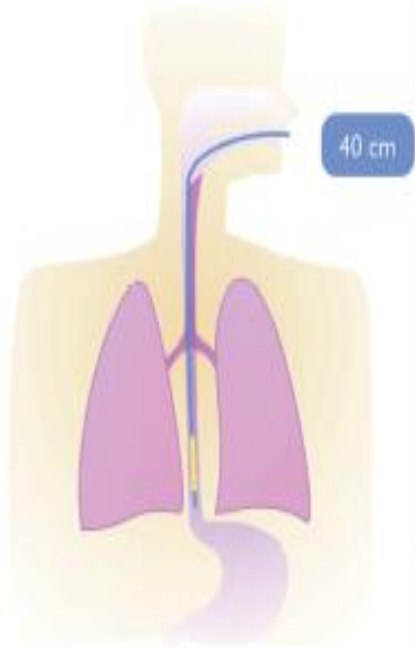


Fig. 6. Left: Correct positioning of the esophageal balloon, ~40 cm from the lips. Center: Chest radiograph showing correct balloon placement (arrow). Right: Note that the esophagus borders the pleural space in the mid-thorax (arrows). Left and center images from Reference 19.

ÖZAFAGEAL (PLEVRAL) VE GASTRİK (ABDOMİNAL) BASINÇLAR

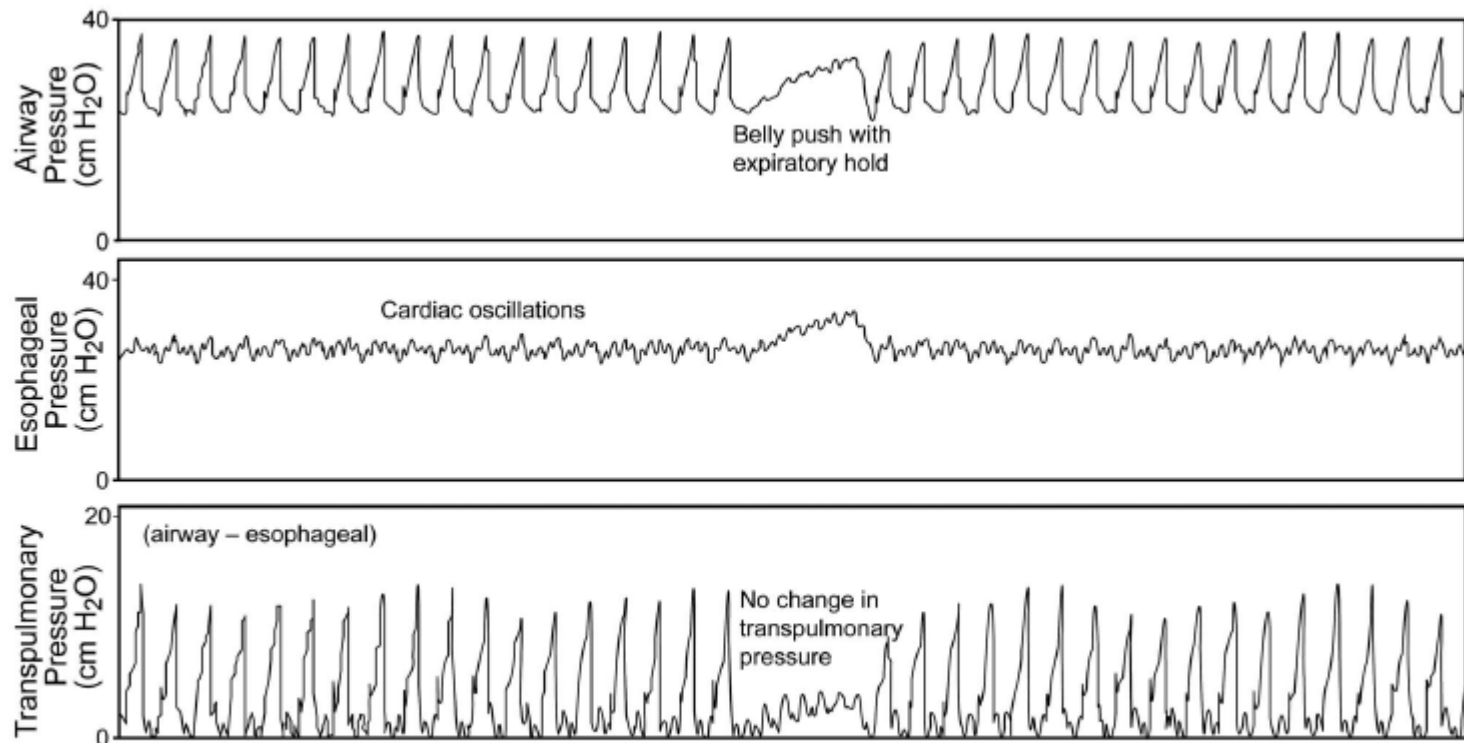


Fig. 5. Illustrated here are several features used to determine that the esophageal balloon is correctly placed in the esophagus. Notice the presence of cardiac oscillations on the esophageal pressure waveform. Also note that there is no change in transpulmonary pressure when pressure is applied to the abdomen.

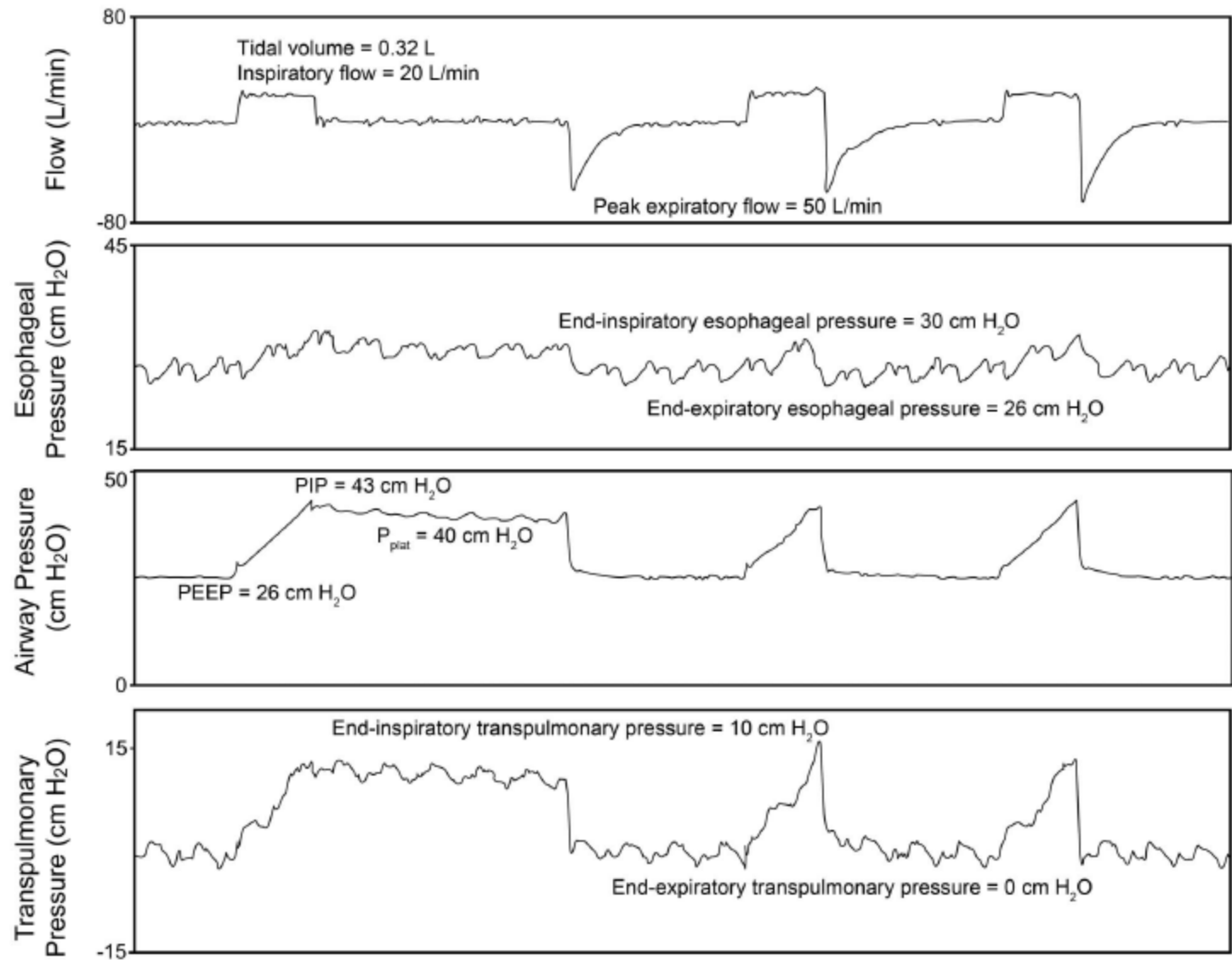


Fig. 17. Flow, esophageal pressure, airway pressure, and transpulmonary pressure can be used to calculate respiratory system compliance, chest-wall compliance, lung compliance, inspiratory airway resistance, and expiratory airway resistance. See text for details. PIP = peak inspiratory pressure; P_{plat} = plateau pressure.

Table 1 Case-scenarios in which esophageal and transpulmonary pressure monitoring could be of help at the bedside

Case-scenario	Relevant Pes-derived measure ^a	Clinical significance	Clinical recommendation
Passively ventilated patient	Tidal ΔP_L	Measure of the tidal stress applied to lung parenchyma	Possibly keep below 10–12 cmH ₂ O in ARDS patients
	End Inspiratory P_L	Measure of the total stress applied to lung parenchyma	Possibly keep below 20–25 cmH ₂ O in ARDS patients
	End expiratory P_L	Negative value possibly indicating tendency of the alveoli and/or airways to collapse	Possibly keep above 0 cmH ₂ O in ARDS patients
	Transmural pulmonary vascular pressure	Effective pressure driving blood flow in intrathoracic vascular structures	Consider delta between CVP and end-expiratory Pes rather than CVP per se to better understand volume status of the patient
	Periodically interspersed negative Pes swings after passively delivered ventilator breaths	Detection of reverse triggering	Consider paralysis or modify sedation (reduce sedation to let the patient trigger)
	Ventilated patient with active breathing	Transmural pulmonary vascular pressure	Effective pressure across intrathoracic vascular structures
End inspiratory P_L		Measure of the tidal stress applied to lung parenchyma	Possibly keep below 20–25 cmH ₂ O in ARDS patients
P_{mus}		Measure of the pressure generated by the patient's inspiratory muscles	Normal values are between 5 and 10 cmH ₂ O
Work of breathing		Measure of patient's total work during the respiratory cycle	Normal values are around 0.35 or 2.4 J min ⁻¹
PTPes		Measure of patient's respiratory muscles effort to breathe	Normal values are around 100 cmH ₂ O s min ⁻¹
Negative Pes swings without ventilator pressurization		Ineffective effort	Titrate PEEP and/or decrease support and/or consider NAVA
Pes inspiratory time longer than ventilator inspiratory time		Double triggering or premature cycling	Increase ventilator Ti up to 0.8–1.0 s or consider switching to NAVA or PAV. Rule out non-ventilatory causes (metabolic acidosis, encephalopathy, etc.)
No Pes swing prior to ventilator pressurization		Auto-triggering	Check for leaks, trigger settings, ventilator tubing (water in circuits) and/or decrease sedation
Increasing PTPes and/or Pes swings along spontaneous breathing trial		High likelihood of failure to wean	Differentiate whether resistive or elastic workload increased and treat consequently. Reconnect to ventilator

ARDS Acute respiratory distress syndrome, CVP central venous pressure, NAVA neurally adjusted ventilatory assist, PAV proportional assist ventilation, PEEP positive end-expiratory pressure, Pes esophageal pressure, P_L transpulmonary pressure, ΔP_L change in transpulmonary pressure, P_{mus} inspiratory muscle pressure, PTPes esophageal pressure–time product, Ti inspiratory time.

^a The end expiratory P_L is the absolute value. The end inspiratory P_L can be measured with the elastance method or the absolute value. They do not give the same results, the absolute value being generally lower

SOLUNUM MEKANİKLERİ

- **Work of breathing**
 - **WOB= P X V** (ventilasyonu gerçekleştirecek akımın başlaması için gereken enerji)

Table 2. – Determinants of work of breathing in ventilator-dependent patients

Patient's abnormal mechanics

Low compliance

High flow resistance

PEEPi

Diameter of the endotracheal tube

Ventilator circuit, valves and devices

Ventilatory pattern

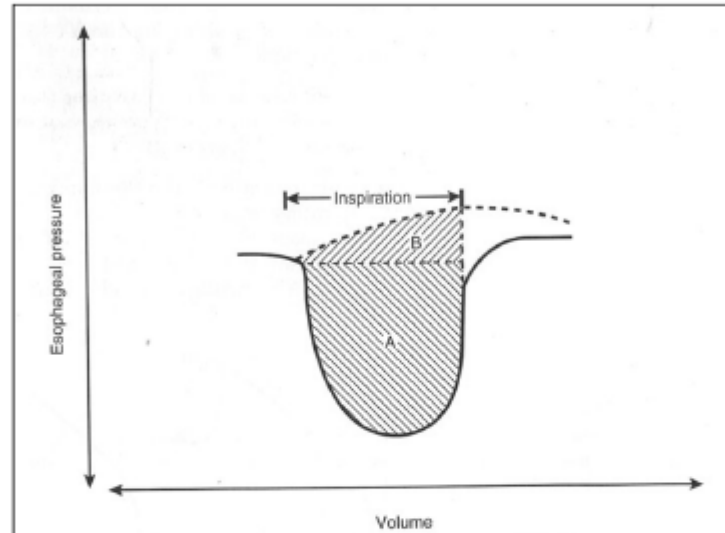
V_T and V_E

Inspiratory flow rate and waveform.

PEEPi: intrinsic positive end expiratory pressure; V_T: tidal volume; V_E: minute ventilation.

SOLUNUM MEKANİKLERİ-WOB

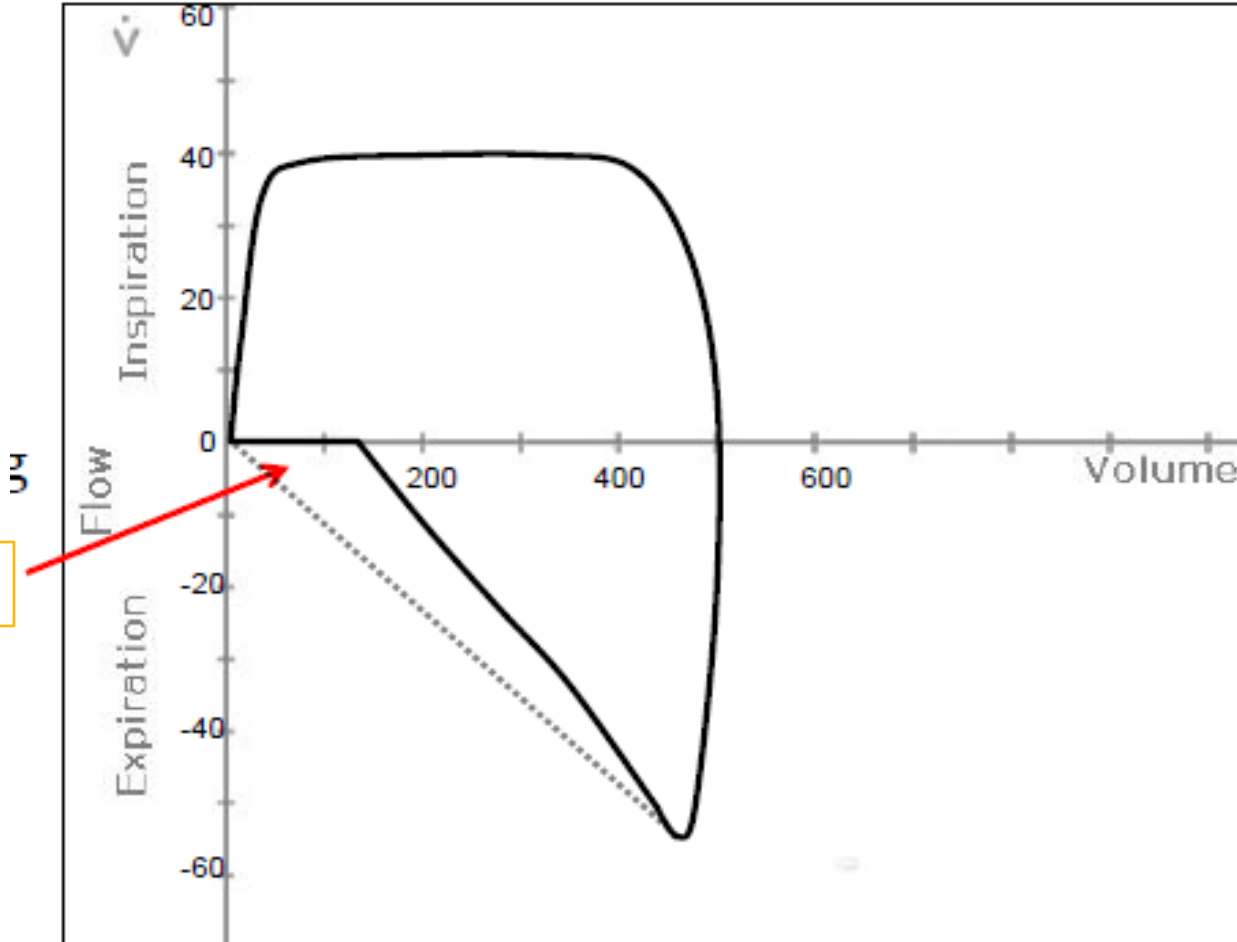
Figure 8



Calculating the work of breathing during spontaneous ventilation using an esophageal balloon. Area A represents the work to move air into and out of the lungs. Area B represents the work to expand the chest wall and is calculated from a pressure-volume curve in a passive patient receiving a mechanically generated breath. The sum of A and B represents the total work of breathing, and it can be determined through integration of the product of esophageal pressure and flow. Reprinted from [1] with permission from Elsevier.

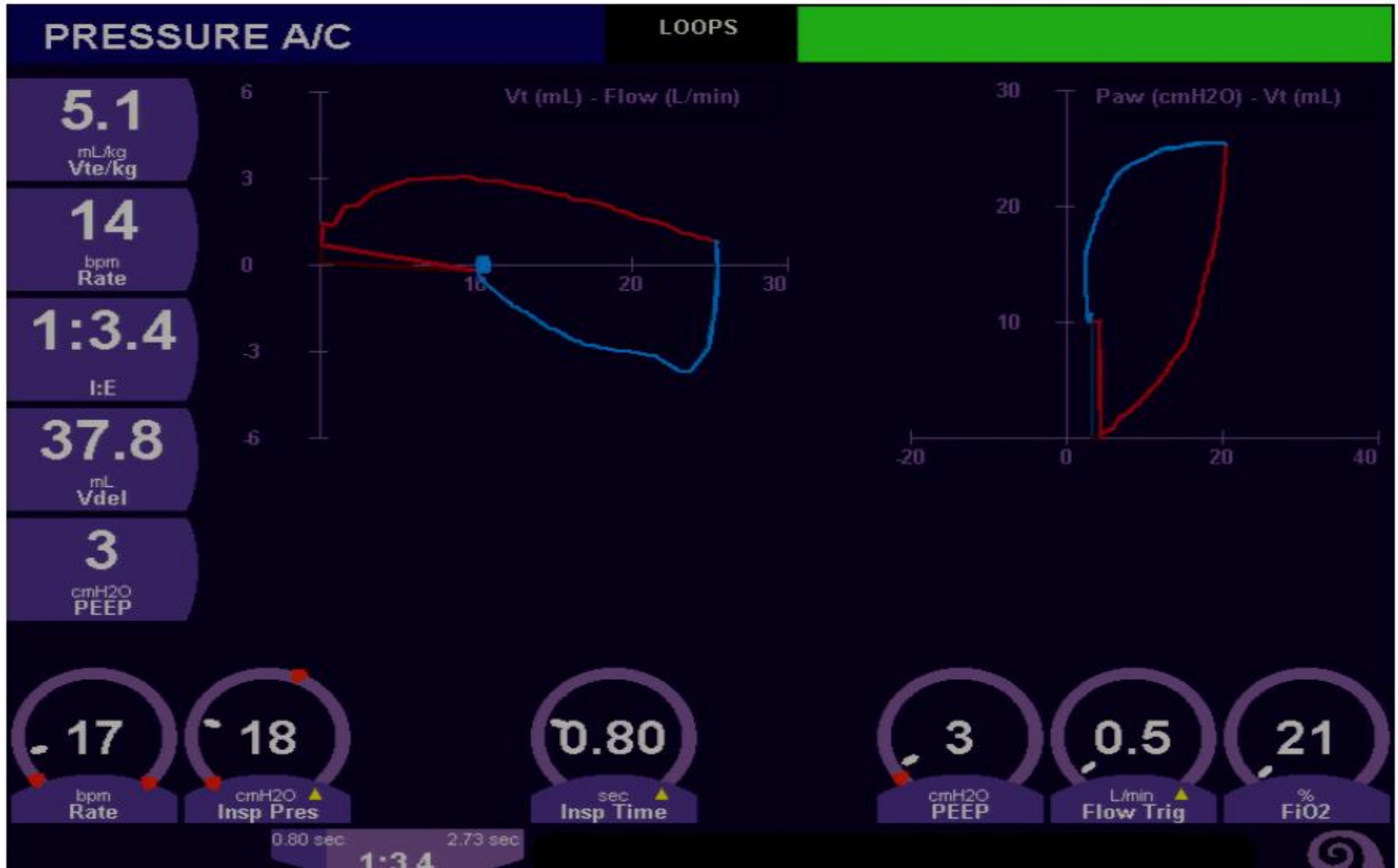
DİĞER ÖZEL BULGULAR

HAVA KAÇAĞI

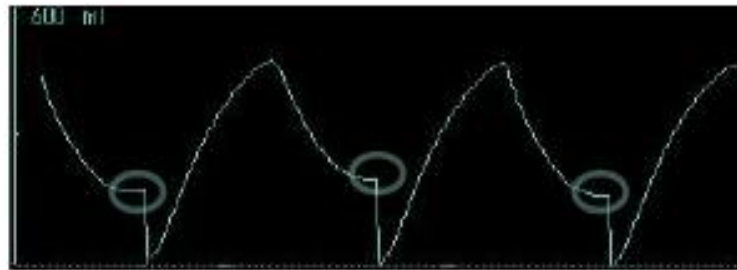
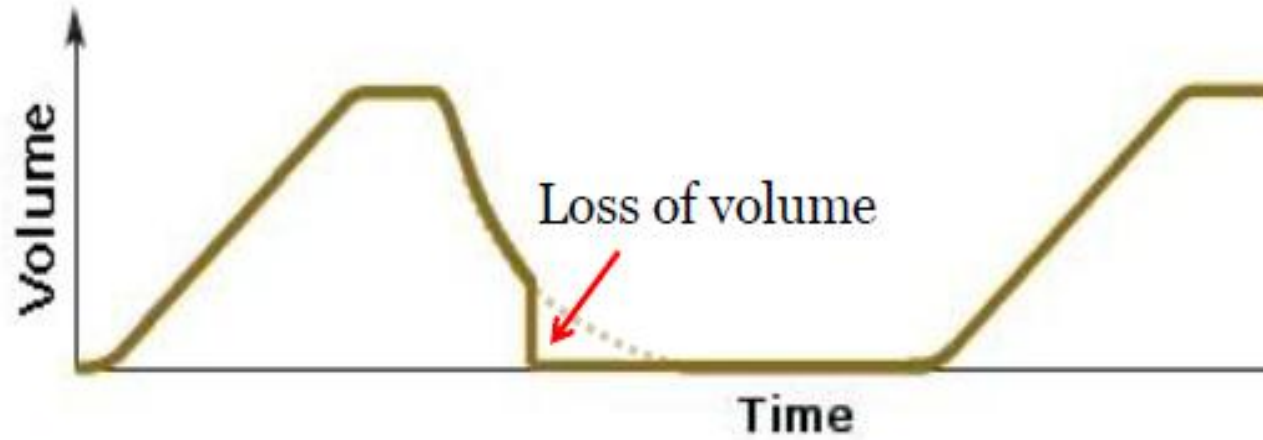


Hava Kaçağı

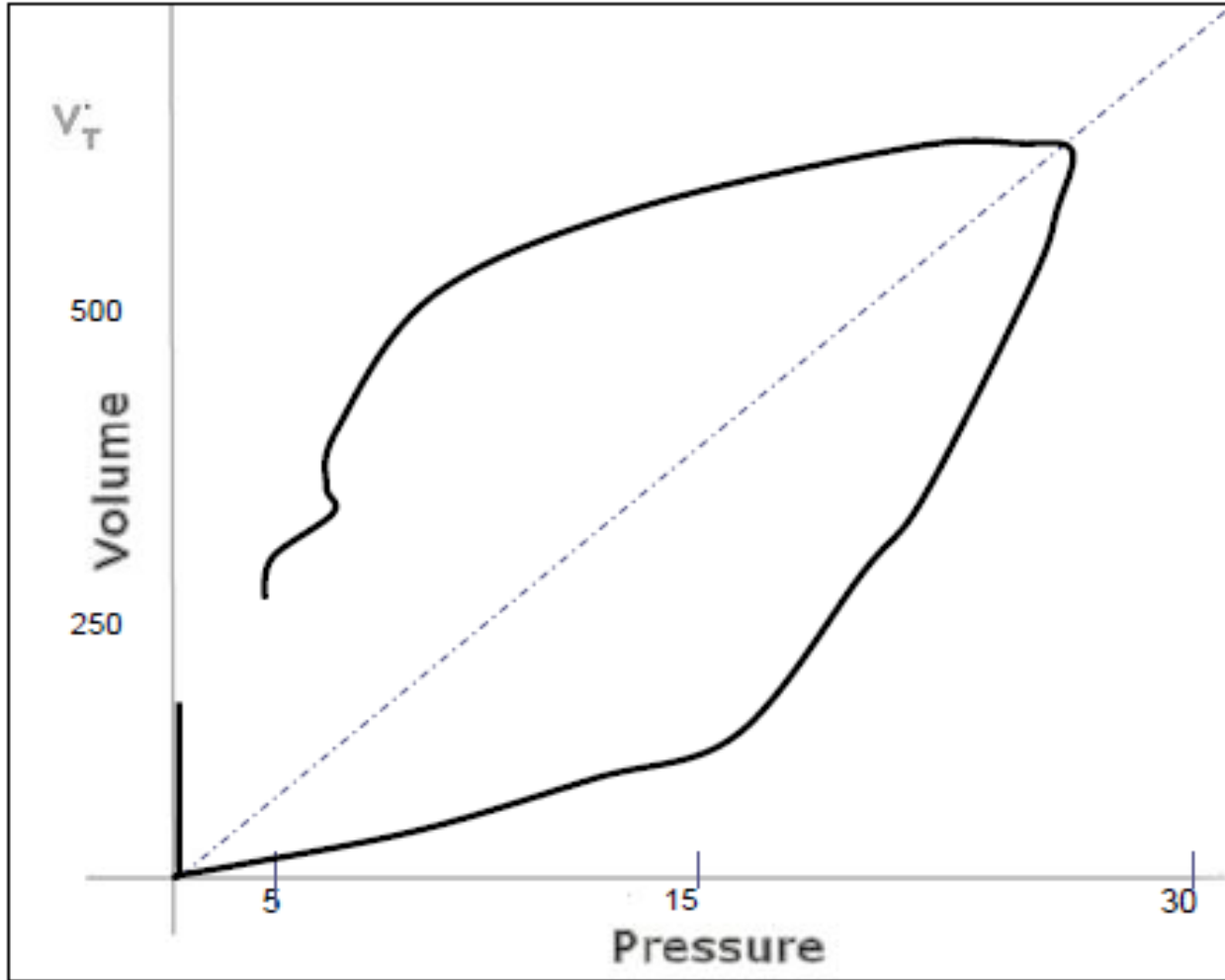
HAVA KAÇAĞI



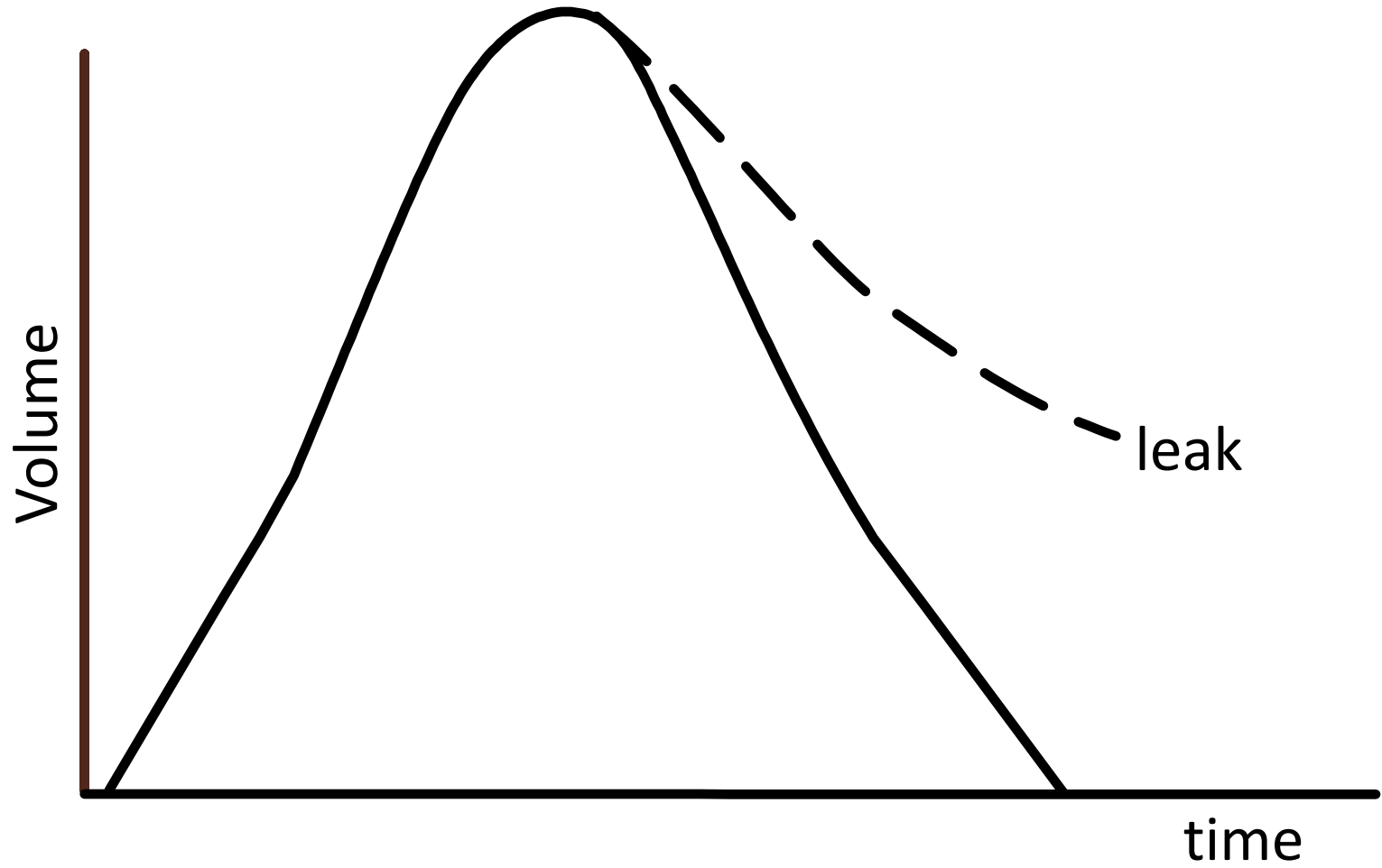
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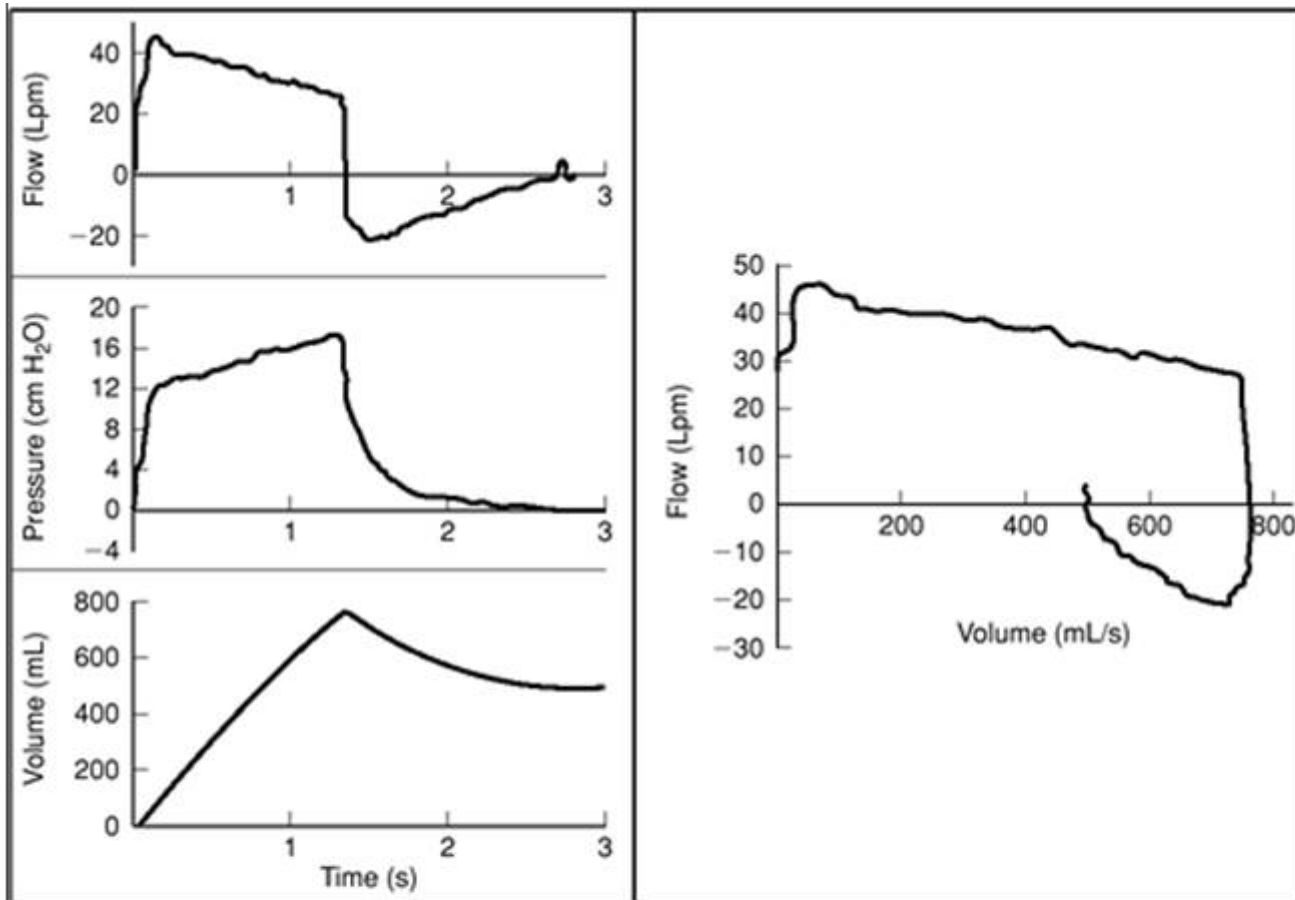
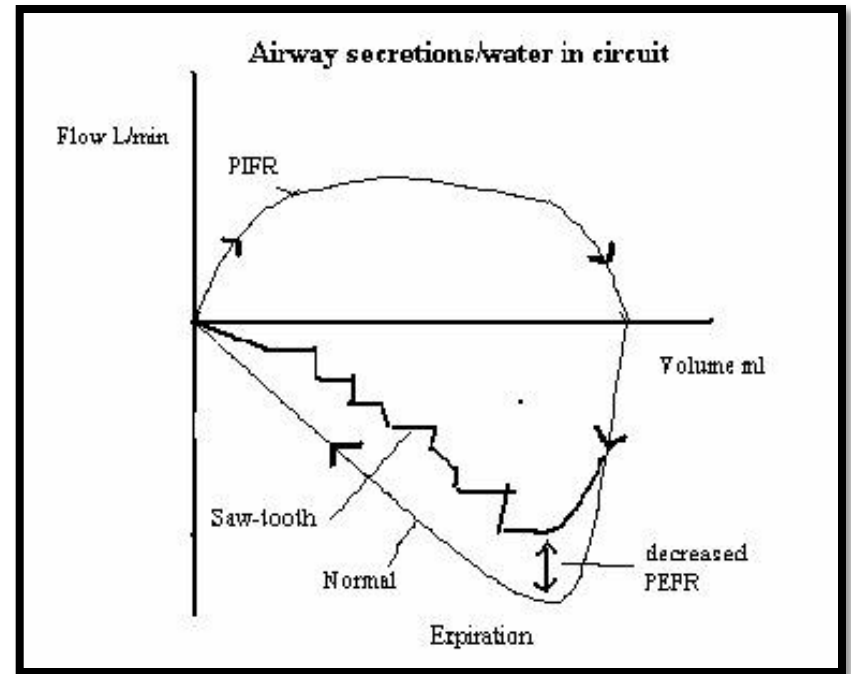
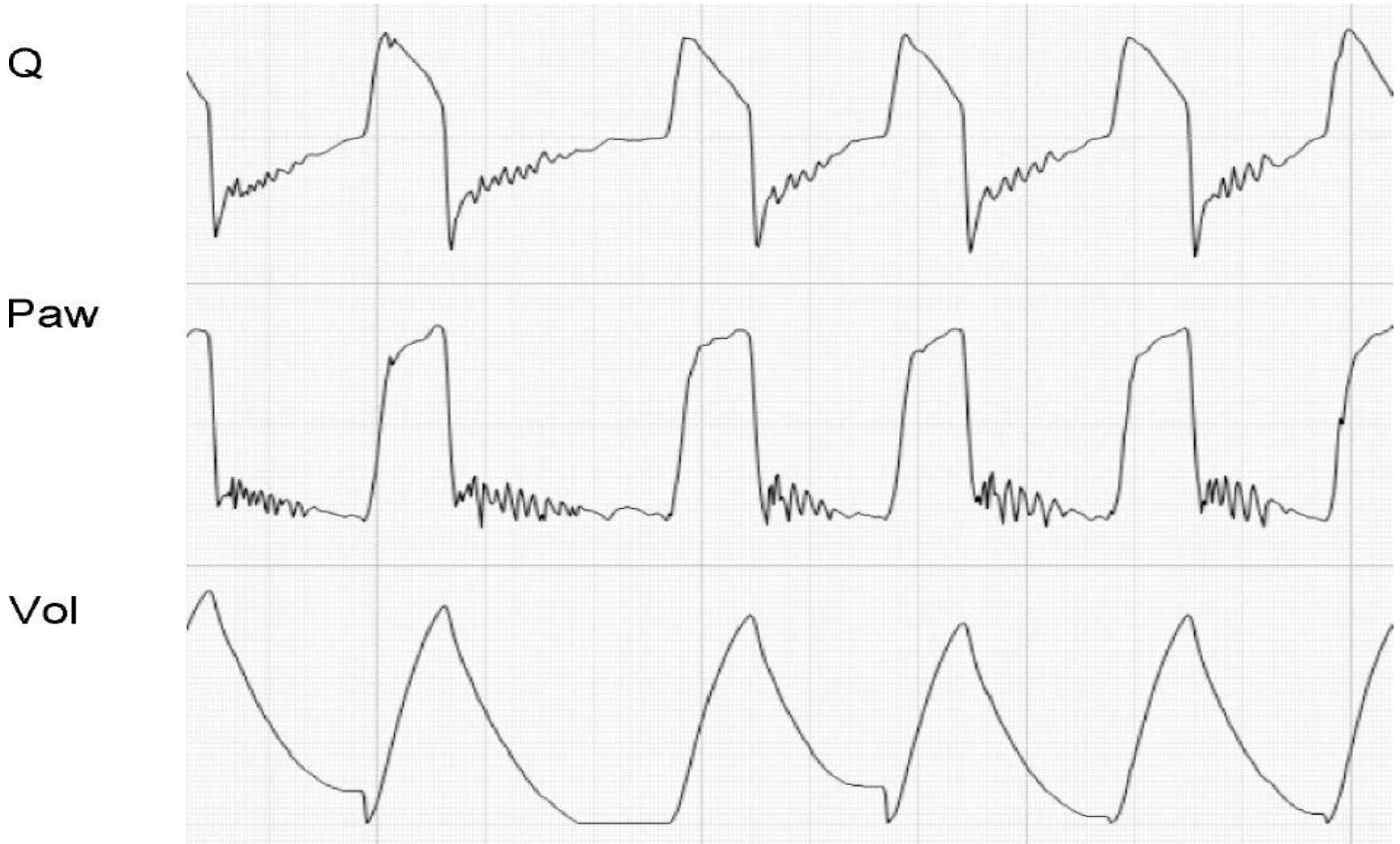


Figure 131.6. Detection of an air leak by ventilator waveform analysis. On the **left**, traces of flow, airway pressure, and volume. Note in the flow trace, the area under the curve (i.e., tidal volume) is smaller during exhalation, indicating a loss of volume. Also note the volume trace that does not reach baseline. On the **right**, the flow–volume loop fails to close at end exhalation. (Modified from Lucangelo U, Bernabe F, Blanch L. Respiratory mechanics derived from signals in the ventilator circuit. *Respir Care*. 2005;50:55–65, with permission.)

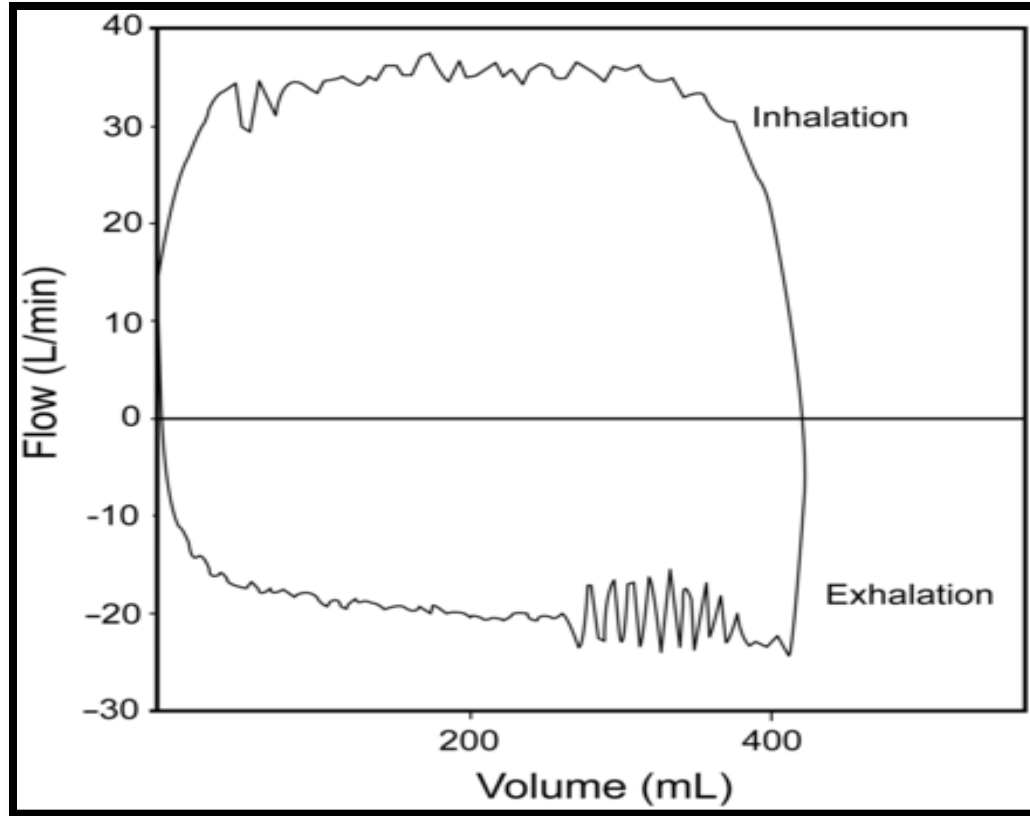
SİSTEMDE SU VEYA SEKRESYON



SİSTEMDE SU VEYA SEKRESYON



ENDOTRAKEAL TÜP SEKRESYON İLE TIKANIRSA



FIX-OBSTRÜKSİYON PATERNİ



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Benim naçiz vücudum elbet bir gün toprak olacaktır, ancak
Türkiye Cumhuriyeti ilelebet payidar kalacaktır.

K. Atatürk

*Saygı ve Özlemle
Anıyoruz*

TEŞEKKÜRLER.....